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2 **Localised cutaneous microvascular adaptation to exercise training**  
3 **in humans**

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37 **Abstract**

38 **Purpose.** Exercise training induces adaptation in conduit and resistance arteries in humans,  
39 partly as a consequence of repeated elevation in blood flow and shear stress. The stimuli  
40 associated with intrinsic cutaneous microvascular adaptation to exercise training have been less  
41 comprehensively studied.

42 **Methods.** We studied 14 subjects who completed 8-weeks cycle ergometer training, with partial  
43 cuff inflation on one forearm to unilaterally attenuate cutaneous blood flow responses during  
44 each exercise-training bout. Before and after training, bilateral forearm skin microvascular  
45 dilation was determined using cutaneous vascular conductance (CVC: skin flux/blood pressure)  
46 responses to gradual localised heater disk stimulation performed at rest (33, 40, 42 and 44°C).

47 **Results.** Cycle exercise induced significant increases in forearm cutaneous flux and  
48 temperature, which were attenuated in the cuffed arm (2-way ANOVA interaction-effect;  
49  $P<0.01$ ). We found that forearm CVC at 42°C and 44°C was significantly lower in the uncuffed  
50 arm following 8-weeks of cycle training ( $P<0.01$ ), whereas no changes were apparent in the  
51 contralateral cuffed arm ( $P=0.77$ , interaction-effect  $P=0.01$ ).

52 **Conclusions.** Lower limb exercise training in healthy young men leads to lower CVC-responses  
53 to a local heating stimulus, an adaptation mediated, at least partly, by a mechanism related to  
54 episodic increases in skin blood flow and/or skin temperature.

55

56 **Keywords:** skin microcirculation; blood flow; exercise training

57

58 **Abbreviations**

59 BMI – body mass index

60 CVC – cutaneous vascular conductance

61 HRMax- Heart rate max

62 PU – Perfusion units

63 SNP – sodium nitroprusside

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## Introduction

Exercise training has strong and independent cardioprotective effects (Blair and Morris 2009) that may be partly mediated through the direct impact of exercise on the vasculature (Green *et al.* 2008; Joyner and Green 2009; Green *et al.* 2017). In conduit and resistance arteries, dynamic exercise training using large muscle groups leads to generalised effects on the vasculature (Thijssen *et al.* 2012; Green *et al.* 2011; Silber *et al.* 1991; Snell *et al.* 1987). For example, cycle ergometer exercise training, which specifically avoided hand-gripping or use of the upper limb musculature, induced brachial artery adaptation (Birk *et al.* 2012; Tinken *et al.* 2008). Interestingly, when exercise-mediated increases in brachial artery blood flow were attenuated during exercise bouts (via unilateral partial cuff inflation), these adaptations were no longer apparent, implying a role for haemodynamic forces, such as shear stress, as important stimuli to conduit artery adaptation in response to exercise training in humans (Birk *et al.* 2012; Tinken *et al.* 2010; Green *et al.* 2017).

Whilst conduit and larger resistance arteries adapt to exercise training by enhancing function and then remodelling to increase their diameter (Green *et al.* 2017; Tinken *et al.* 2008; Laughlin 1995), studies of microvascular adaptation in skeletal muscle have proposed that increases in capillarity in response to training may counteract reductions in red cell transit time, enabling increased oxygen extraction (Krustrup *et al.* 2004). In this context, it is well established that the mode of adaptation to training differs according to rank order along the arterial tree; larger arteries primarily respond to shear stress and other hemodynamic stimuli via cross sectional enlargement (Rowley *et al.* 2011; Newcomer *et al.* 2011), whereas microvessels respond to these

stimuli (and hypoxia) by budding and sprouting (Cocks *et al.* 2013; Andersen and Henriksson 1977; Brown 2003).

The role of repeated exercise and shear stress in the adaptation of cutaneous microvessels is less well understood, despite the obvious relevance of changes in the structure and function of these vessels to microvascular disease (Simmons *et al.* 2011; Holowatz *et al.* 2008). Some evidence suggests that exercise training induces intrinsic adaptation in the cutaneous microvasculature (Black *et al.* 2008; Simmons *et al.* 2011), whilst we recently completed a series of studies, involving repeated localised and systemic heating, which suggested that cutaneous microvascular adaptation may depend upon local skin temperature changes in addition to changes in blood flow and shear stress that occur as a consequence of elevation in core temperature (Green *et al.* 2010; Carter *et al.* 2014). The contribution of these important physiological stimuli to cutaneous adaptation in response to leg exercise training is currently unknown.

The primary aim of this study was to examine the role played by repeated increases in blood flow in localised adaptations in the skin microcirculation of the upper limbs, following 8-weeks of cycling exercise. To address this aim, we partially inflated a pneumatic cuff around one forearm during each exercise bout, to unilaterally attenuate exercise-induced hyperaemia (Tinken *et al.* 2009; Tinken *et al.* 2010). Before and after the intervention, skin blood flow responses were assessed at rest using a local heating protocol. We chose to use a localised disk heating protocol as a tool to assess intrinsic microvascular adaptation in the skin because it is well established that this approach provides an intrinsic microvascular index that is independent of reflex neurovascular control (Minson *et al.* 2001; Black *et al.* 2008). We hypothesised that cycle

exercise training, by inducing repeated episodic increases in cutaneous blood flow would increase forearm skin vasodilator capacity in response to a localised heating stimulus.

## **Materials and Methods**

### **Ethical Approval**

All study procedures complied with the *Declaration of Helsinki* and were approved by the Human Research Ethics Committee at Liverpool John Moores University and The University of Western Australia. All subjects provided written, informed consent before participating in the study.

### **Subjects**

Fourteen healthy men (Age:  $25 \pm 2$  years, Height:  $180 \pm 5$  cm, Weight:  $76 \pm 13$  kg and BMI:  $23 \pm 3$  kg.m<sup>-2</sup>) were recruited to participate in an exercise training experiment. A further 6 male subjects ( $27 \pm 6$  years) undertook an acute cycle exercise experiment to characterise forearm skin blood flow changes. No subject had cardiovascular disease, diabetes, insulin resistance or possessed cardiovascular risk factors such as hypercholestaemia or hypertension. Subjects who smoked or were on medication of any type were excluded. Participants at pre-study entry were either classified as sedentary or recreationally active (<5 hours per week). All sedentary participants only took part in the prescribed 3 x 30 min sessions per week across the 8 weeks and no new activity was introduced outside of this. All recreationally active participants were asked to keep their activity levels consistent throughout the 8 week intervention so that the additional 3 x 30 mins a week were in addition to pre-entry exercise levels.

**Acute experiment (n=6): Effect of leg cycle exercise on skin microvascular responses  $\pm$  forearm cuff inflation**

Participants undertook 30 mins of cycle exercise (Monark 874E, Sweden) at 80% HRmax (age-predicted). Throughout the exercise bout a pneumatic cuff (6cm in width: SC5D Hokanson cuff, Bellevue USA) was placed around one forearm immediately below the cubital crease and inflated to 60mmHg. Previous studies have demonstrated that placement and inflation of a forearm cuff in this manner attenuates brachial artery blood flow (Birk et al. 2012; Thijssen et al. 2009; Tinken et al. 2010; Tinken et al. 2009). The contralateral arm remained uncuffed during the exercise bout. Subjects rested for 10-mins on the ergometer in a quiet, temperature controlled room. Baseline bilateral forearm skin blood flows using laser-Doppler flowmetry (Model 413, Periflux 5001 System, Perimed AB) were then recorded for 2.5 mins, followed by unilateral cuff inflation to 60 mmHg for 2.5 mins. Skin blood flow data were recorded in both arms on the ventral side of the forearm during the exercise bout and averaged in 2.5-min bins along with skin temperature using thermistors (Squirrel 1000 series, Grant Instruments, Cambridge, United Kingdom). Placement of skin thermistors and laser Doppler probes was the same on both arms and always distal to the cuff site. In order to avoid any instances of handgripping, participants were instructed to rest both arms on the handle bars of either side of the bike.

**Chronic experiment (n=14): Effect of leg cycle exercise on skin microvascular responses  $\pm$  forearm cuff inflation**

Exercise training was performed over an 8-week period with subjects visiting the laboratory 3 times per week. Each of these 24 sessions was supervised and consisted of 30 mins of cycle

exercise (80% age-predicted HRmax, cadence 60 rpm), performed at the same time of day. As above, a pneumatic blood pressure cuff was placed below the cubital crease on one forearm of each subject and inflated to 60 mmHg throughout each 30 min exercise training bout. The arm selected for cuff placement was randomised, but once selected, it remained consistent across the 8-week training period for any given participant.

### ***Gradual local heating protocol***

Assessments were performed before and after the 8-week cycling exercise training program at rest. All studies were conducted in a quiet, temperature controlled environment and each visit for a given subject was performed at the same time of day. Subjects were asked to fast for 8 hours, abstain from alcohol and caffeine for 16 hours, and not to perform any exercise for 24 hours. Probe placement sites were selected on each forearm and the location of these sites was recorded using photographs and distances from anatomical landmarks, so that repeated measures were collected at the same skin site. In a previous study, we examined the day-day reproducibility of forearm skin responses to our local heating protocol. Coefficients of variation of 17.1 and 14.4% were obtained when skin responses were presented as absolute cutaneous vascular conductance (CVC; at 42 and 44°C, respectively) (Dawson et al. 2015).

Upon arrival, subjects were seated and instrumented for ~20 mins before beginning the ~90 min heating protocol. Local heater disks (Perimed 455, Stockholm, Sweden) were placed on the forearms using double-sided adhesive rings. The laser Doppler probes, each with a 7-laser array (Model 413, Periflux 5001 System, Perimed AB), were then fitted into the middle of these localised heating disks to record change in red blood cell flux (in perfusion units, PU)



(Cracowski et al. 2006). Once instrumented, recording commenced and the heater disk temperatures were increased to 33°C and maintained at this temperature for a 10 min baseline period. Upon completion of this baseline period, increments in heater disk temperature were gradual, so as to minimise the influence of the axon reflex on the skin blood flow response (Minson et al. 2001). Heat increased in controlled increments of 0.5°C every 2.5 mins until 42°C was reached. Once the probes reached 42°C, they remained at this temperature for a period of 30 mins. Finally, heater disk temperatures were increased to 44°C for another 20 mins to induce a maximal skin blood flow response. Previous studies have suggested that heating to the levels used in the present study results in similar CVC increases to those observed in response to infusion of SNP (Kellogg et al. 1999; Cracowski et al. 2011), indicating that maximal responses are indeed obtained and that these reflect the structural capacity of the microvasculature. Resting blood pressure was recorded every 15 min using an automated sphygmomanometer placed around the ankle (Dinamap; GE Pro 300V2, Tampa, FL). Blood pressure measures taken at the ankle were later corrected for the hydrostatic column by multiplying the vertical height difference between the right atrium and the ankle (cm) by 0.766 to convert to mmHg (Groothuis et al. 2008), this value was then subtracted from the raw blood pressure value acquired at the ankle. Converted blood pressure values were then used to calculate CVC, which accounts for skin blood flow changes occurring as a result of changes in blood pressure (Cracowski et al. 2006). All laser Doppler measurements were relayed and graphed in real time via a Powerlab onto a laptop running LabChart 7 (AD Instruments, Sydney, Australia).

### **Data analysis and statistics**

Skin blood flow (PU) from the cuffed and uncuffed arms was averaged across 1-minute intervals. Calibration of the laser Doppler probes was undertaken before and after the experiments using two generic points, 0 and 250 PU, in accordance with calibration guidelines using a zeroing disk and motility standard (Periflux System, Perimed AB). We measured and analysed the 2.5 min increment at 40°C, as well 5-min averages of data from the plateau-phases at 42°C and 44°C. Measurements in PU were converted to CVC which was calculated as PU/Dinamap mean arterial pressure (MAP).

Statistical analyses were performed using SPSS 21.0 (SPSS, Chicago, Illinois) software. All data are reported as mean (SD) unless stated otherwise, while statistical significance was assumed at  $P \leq 0.05$ . Initially, a linear mixed model was conducted (with time and cuff inflation as factors) for both skin temperature and skin blood flow during the acute study. A second linear mixed model was used with local heating (33, 40, 42 and 44°C) and time (Week 0 & 8) as factors in order to assess change in CVC responses to the 8-week intervention in the uncuffed and cuffed arm. Finally, a linear mixed model was performed on delta change CVC scores (Week 8 minus Week 0) with cuff and heating as factors. Post-hoc analysis was performed using the least significant difference (LSD) method for pair-wise multiple comparisons when a significant main effect was observed (Perneger 1998).

## Results

### **Acute experiment (n=6): Effect of leg cycle exercise on skin microvascular responses $\pm$ forearm cuff inflation**

Results of a linear mixed model revealed that heart rate increased significantly during the leg cycling exercise bout (Figure 1A). The increase in HR observed prior to exercise from the -2.5 to 0 min time points may be attributable to an anticipatory response (Williamson et al. 2006). Skin temperature in the uncuffed forearm increased modestly, but significantly, during exercise (by 1.8°C, Figure 1B). However, no change in skin temperature was observed during leg cycling exercise in the cuffed arm (Figure 1B). No significant differences were evident in skin blood flow between the cuffed and uncuffed arms in the baseline period before the cuff was inflated (13.1 $\pm$ 3.5 vs. 15.5 $\pm$ 9.1 PU, respectively,  $P=0.41$ ). After the onset of leg cycling exercise, there was a significant increase in skin blood flow in the uncuffed arm, whilst the increase in flow was significantly attenuated in the cuffed arm (linear mixed model; interaction effect between exercise and cuff inflation of  $P<0.01$ , Figure 1C).

### **Chronic experiment (n=14): Effect of leg cycle exercise on skin microvascular responses $\pm$ forearm cuff inflation**

Across the 8-week exercise training period, there was 97% adherence to the training sessions in the 14 subjects. The efficacy of our training intervention is indicated by a decrease in the average resting heart rate after 8 weeks of cycle exercise training (67 $\pm$ 11bpm vs. 58 $\pm$ 9; t-test:  $P=0.01$ ). In addition, to maintain exercise HR at 80% HR<sub>max</sub>, the workload performed in the exercise sessions increased significantly over the 8 weeks of training, from 129 $\pm$ 19W to

154±21W at week 8 ( $P<0.01$ ). Resting MAP did not change after training ( $89\pm 8$  vs  $88\pm 6$  mmHg,  $P=0.57$ ).

### ***Gradual local heating protocol***

Figure 2 shows a representative response to local heating in one subject throughout the temperature increments while Figure 3 presents the responses to our local heating protocol before and after training in the cuffed and uncuffed arms. Figure 3 presents CVC data in absolute values, rather than normalised to the peak ( $44^{\circ}\text{C}$ ) maximum. This is because we wished to understand whether the peak responses *per se* were elevated, possibly indicative of changes in microvascular capacity. Values for CVC at baseline ( $33^{\circ}\text{C}$ ), heating ( $40^{\circ}\text{C}$ ) and during the plateau at  $42^{\circ}\text{C}$  and  $44^{\circ}\text{C}$ , in the cuffed and uncuffed limbs were similar prior to training ( $P$ -values: 0.32, 0.74, 0.51 and 0.76, respectively). A linear mixed model revealed a significantly lower CVC following training at  $42^{\circ}\text{C}$  and  $44^{\circ}\text{C}$  (Figure 3A) in the uncuffed arm (interaction effect  $P=0.01$ , time effect  $42^{\circ}\text{C}$   $P\leq 0.01$ , time effect  $44^{\circ}\text{C}$   $P\leq 0.01$ ). However, in the contra-lateral cuffed arm, CVC did not change as a result of training (Figure 3B) (interaction effect  $P=0.69$ ). A linear mixed model for changes in CVC (expressed as CVC Week 8 minus CVC Week 0) between uncuffed vs. cuffed revealed a significant effect for cuff inflation ( $P<0.01$ ).

## **Discussion**

The aims of the present study were to describe the impact of cycle exercise training on maximal forearm skin blood flow responses to local heating and to determine whether adaptations were dependent upon repeated exposure to increases in blood flow. Our experimental manipulation,

involving partial cuff inflation on one arm, was successful in unilaterally manipulating forearm skin blood flow and temperature during leg exercise. Our principal finding, in contrast to our hypothesis, is that cycle exercise training significantly decreased forearm CVC-responses to local heating in the uncuffed forearm. Our findings suggest that this adaptation was mediated by repeated increases in skin blood flow and/or temperature, as no changes were observed in the cuffed forearm which was exposed to significantly lower levels of blood flow/temperature during each cycle exercise training session (Figure 1).

Elicitation of skin blood flow responses via local heating is commonly used for assessment of the cutaneous vasculature (Boignard *et al.* 2005; Minson *et al.* 2002; Smith *et al.* 2011; Colberg *et al.* 2005). However, few studies have focussed on modification of the localised cutaneous microvasculature following exercise training in humans (Boegli *et al.* 2003; Black *et al.* 2008). Previous studies by our group have utilised exercise-independent interventions to determine the role of repeated increases in skin blood flow on cutaneous vascular function, and found that episodic increases in flow are obligatory for enhanced responsiveness to the local heating test above (Green *et al.* 2010; Carter *et al.* 2014). It is also well documented that repeated increases in shear stress act as a potent stimulus for improved endothelial vascular adaptation and NO availability in larger conduit and resistance arteries in humans (Hambrecht *et al.* 2003; Tinken *et al.* 2010). These findings informed the rationale for the present study, in which exercise training was used as a stimulus, but the changes in forearm blood flow and shear stress associated with cycle exercise were clamped unilaterally.

No previous study has attempted to investigate the role of repeated increases in blood flow on

skin vessels following an exercise intervention. We hypothesised that cycle exercise training would increase skin blood flow responsiveness to local heating, an adaptation mediated by repeated increases in skin blood flow and/or temperature, consistent with the studies above (Green *et al.* 2010; Carter *et al.* 2014). On first pass, our finding in the current study of lower peak CVC responses following the intervention suggests that exercise training may have decreased the release of vasodilator stimuli in response to local heating. However, the skin circulation is highly complex, governed by a number of local and systemic mechanisms (Charkoudian 2003), and the possibility that exercise training induces decreased microvascular function seems unlikely. Moreover, the responses to sustained skin heating to 44°C provide an index of peak microvascular vasodilation, commonly used as an index of structural, rather than functional, vascular adaptation in humans (Kellogg *et al.* 1999; Choi *et al.* 2014; Johnson *et al.* 1986; Taylor *et al.* 1984; Green *et al.* 1994). Of interest, a recent study by Brunt *et al.* (Brunt *et al.* 2016) involving repeated whole body heating for 8 weeks induced improvements in local skin vascular function, but non-significant *decreases* in maximal local heating responses (5.5% decrease in CVC<sub>max</sub>), consistent with our data. Collectively, these findings argue against the notion that our findings infer detrimental functional adaptations in the skin microvessels and that, rather, they may reflect changes in microvascular structure.

The possibility that exercise training induces structural adaptations in the skin microcirculation is supported by established findings in both resistance and conduit arteries, that exercise training induces arterial remodelling and structural arterial enlargement (Haskell *et al.* 1993; Naylor *et al.* 2005; Green *et al.* 1994; Rowley *et al.* 2011; Tinken *et al.* 2008). Such findings are supported by extensive animal literature (Langille and O'Donnell 1986). In the current study, the decrease in

absolute values for CVC that we observed in the uncuffed arm is not likely to be the result of a decrease in total blood flow to the forearm, since resting brachial artery blood flow [published in (Birk *et al.* 2012)] did not decrease after 8 weeks cycle exercise training ( $43.3 \pm 20.2$  vs  $57.0 \pm 28.5$  mL/min,  $P=0.14$ ). We therefore speculate that the decrease in skin flux that we observed following training in response to local skin heating may reflect enlargement of microvessels and/or an increase in the number of capillaries, in that larger microvascular beds should be associated with prolonged red cell transit time. Whilst we admit that such structural adaptation is a novel and speculative proposal in terms of the human cutaneous vasculature, some supportive evidence for microvascular adaptation after exercise training is provided by studies of skeletal muscle capillary density (Fernandes *et al.* 2012a; Fernandes *et al.* 2012b). Indeed, it has been suggested that increased microcirculatory volume in skeletal muscle following exercise training would counteract higher muscle blood flows, allowing sufficient time for extraction of oxygen (Krustrup *et al.* 2004). In support of this notion, Glieman *et al.* observed a training-induced increase in skeletal muscle capillary to fibre ratio as well as increases in capillary lumen area (Gliemann *et al.* 2015). These interesting findings in skeletal muscle suggest that whilst larger (conduit and feed) arteries adapt both functionally and structurally to increase flow (Green *et al.* 2017), there may be simultaneous changes in the microvessels that favour prolongation in red blood cell transit time to optimise gas exchange. This is consistent with our findings and the suggestion, albeit speculative at this stage, that skin adaptation to exercise or whole body heating may induce structural adaptations that are reflected as diminished maximal flux and CVC responses. Whilst changes in microvascular morphology in skeletal muscle may act to prolong transit time and enhance gas exchange, similar adaptation in the human skin would have the

effect of enhancing heat exchange. Further studies should examine these hypotheses and the suggestion that exercise training modifies cutaneous microvascular morphology in humans.

Our finding that changes in CVC were only present in the limb that was exposed to repeated increases in blood flow, infers that shear stress may be an important stimulus for adaptation in human microvessels. Although shear stress decreases during passage down the arterial tree, it is nonetheless likely that the vessels imaged in the present study are exposed to physiologically relevant increases in levels of flow and shear in response to exercise. *In vitro* animal studies have reported that coronary arterioles between 80-130 $\mu\text{m}$  dilated by 50% and arterioles between 25-70 $\mu\text{m}$  dilated by 20-30% in response to shear stress (Kuo *et al.* 1995). The vessels imaged in this study are likely >30-50 $\mu\text{m}$  in diameter (Fredriksson *et al.* 2009; Braverman 1989). Also, Laughlin *et al.* reported that arterioles of smaller size possess more eNOS protein than those >50 $\mu\text{m}$  (Laughlin *et al.* 2003). Regardless of the magnitude of shear the skin microcirculation was exposed to, blood flow through these areas was significantly increased, and this is associated with increased haemodynamic forces, that can act as mediators of adaptation (Brown 2003).

*Limitations.* Cuff inflation to 60mmHg was used to primarily attenuate blood flow in one limb during the exercise bouts. It is conceivable that cuff inflation may have induced unilateral venous distension which, in turn, elicited a reflex cardiovascular response impacting upon skin perfusion or flow (Cui *et al.* 2012). For example, previous studies that have inflated a cuff to 250mmHg and subsequently distended the veins via infusion, have reported a systemic reflex sympathetic impact (Cui *et al.* 2011; Cui *et al.* 2009; Cui *et al.* 2012). If such a reflex was induced in the present experiment, it might explain the contralateral uncuffed limb responses we observed.



However, our experimental design was different to these studies because it involved cuff inflation to just 60 mmHg. Nonetheless, we performed a sub-study to determine potential systemic effects of unilateral cuff inflation to 60mmHg for 30 minutes (n=5). We observed no effects on blood pressure, HR or skin blood flows in the contralateral limb. We therefore think it unlikely, in this particular experiment, that the effects of cuff inflation could drive a large sympathetic response that would induce adaptation in contralateral skin blood flow responses, at rest, to local heating pre- versus post-training. Furthermore, any central reflex effect, if apparent, would manifest in both arms, cancelling out the likely impact in terms of our experimental design. If a unilateral vasoconstrictor reflex was evident in just the cuffed limb as a result of venous distension, then the microvascular adaptation to repeated episodic vasoconstriction should have been greater in the cuffed arm, yet the opposite was the case in this study. We observed no changes in skin microvascular responses to local heating at rest in the arm that had undergone cuffing during the training intervention (Figure 2 and 3). We therefore suggest that elicitation of reflex responses cannot explain the differences we observed between limbs. Another limitation is that we did not examine core temperature responses during acute cycle exercise, before and after exercise training. We cannot, therefore, relate our findings to changes in thermoregulatory capacity, but this was not our aim. The purpose of our study was related to intrinsic adaptations in cutaneous responses following exercise training, and the role of blood flow and temperature in such localised adaptations, which may be relevant to microvascular health and disease. A further limitation relates to our subject group selection. Whilst we studied subjects who were either sedentary or recreationally active (all <5 hrs regular exercise per week), we cannot exclude the possibility that more active or fit subjects may have exhibited different outcomes. Finally, the local heating protocol employed in the present study was not identical to

that used by Black *et al.*. Whilst the rate of temperature increase has been shown to have little effect on the absolute peak skin blood flow response (Choi *et al.* 2014), we cannot entirely rule out the possibility that the use of a different local heating protocol may have induced distinct results to our study.

## **Conclusion**

We found that cycle exercise training decreased forearm skin blood flow responses to localised heating. This adaptation appears to be dependent upon repeated increases in blood flow during exercise bouts, as adaptation in the skin microcirculation was not apparent in the contralateral limb in which flow responses and skin temperature were attenuated via cuff inflation. We speculate that an increase in cutaneous red cell transit time may result from structural adaptations that, correspondingly, lower maximal CVC responses. Although we cannot provide a definitive evidence mechanism for such an adaptation at this stage, due to methodological limitations with the direct assessment of cutaneous microvascular structure, future studies utilising advanced imaging technology (Carter *et al.* 2016) may be able to test this proposal.

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**Figure Legends.**

**Figure 1.** Heart rate (A, in beats per minute), and forearm skin temperature (B, in °C) and skin blood flow (C, in perfusion units (PU)) in the uncuffed (solid squares) and cuffed arm (open squares) before and during cycle exercise (at 2.5-min intervals) in healthy, young volunteers (n=6). Post-hoc significantly different at  $P < 0.05$  from baseline (\*) or between the cuffed and uncuffed arm (#). Error bars represent SE.

**Figure 2.** A representative response of skin blood flow change presented as cutaneous vascular conductance (CVC) during the gradual local heating protocol in the uncuffed (A) and cuffed (B) arms at Weeks 0 and 8 of the exercise intervention. PU: perfusion units; MAP: mean arterial pressure.

**Figure 3.** Forearm skin cutaneous vascular conductance (CVC) at baseline (33°C) and during gradual heating. Submaximal heating (40°C), 42°C (Plateau) and 44 °C (Max) are presented in the uncuffed (panel A) and cuffed arms (panel B) at 0 and following 8 weeks of exercise training (black and white bars, respectively) in healthy, young volunteers (n=14). Post-hoc significantly different at  $P < 0.05$  from baseline (\*). Error bars represent SE.