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Moving forward with backwards compatibility: Translating wrist accelerometer data

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- 4 Short title: Translating wrist accelerometer data
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26 Abstract

27 **Purpose:** To provide a means for calibrating raw acceleration data from wrist-worn 28 accelerometers in relation to past estimates of children's moderate-to-vigorous 29 physical activity (MVPA) from a range of cut-points applied to hip-worn ActiGraph 30 data. Methods: This is a secondary analysis of three studies with concurrent 7-day 31 accelerometer wear at the wrist (GENEActiv) and hip (ActiGraph) in 238 children 32 aged 9-12 years. The time spent above acceleration (ENMO) thresholds of 100, 150, 33 200, 250, 300, 350 and 400 mg from wrist acceleration data (<5 s epoch) was 34 calculated for comparison to MVPA estimated from widely used children's hip-worn 35 ActiGraph MVPA cut-points (Freedson/Trost 1100 counts per minute (cpm); Pate 36 1680 cpm; Evenson 2296 cpm; Puyau 3200 cpm) with epochs of <5, 15 and 60 s. 37 **Results:** The optimal ENMO thresholds for alignment with MVPA estimates from 38 ActiGraph cut-points determined from 70% of the sample and cross-validated with 39 the remaining 30% were: Freedson/Trost = ENMO 150+mg, irrespective of 40 ActiGraph epoch (ICC>0.65); Pate = ENMO 200+ mg, irrespective of ActiGraph 41 epoch (ICC \geq 0.67); Evenson = ENMO 250+ mg for \leq 5 s and 15 s epochs (ICC \geq 0.69) 42 and ENMO 300+ mg for 60 s epochs (ICC=0.73); Puyau = ENMO 300+ mg for <5 s 43 epochs (ICC=0.73), ENMO 350+ mg for 15 s epochs (ICC=0.73), ENMO 400+ mg 44 for 60 s epochs (ICC=0.65). Agreement was robust with cross-validation ICCs=0.62-45 0.71 and means within 17.81±4.9% of MVPA estimates from ActiGraph cut-points, 46 except Puyau 60 s epochs (ICC=0.42). Conclusion: Incremental ENMO thresholds 47 enable children's acceleration data measured at the wrist to be simply and directly 48 compared, at a group level, to past estimates of MVPA from hip-worn ActiGraphs 49 across a range of cut-points.

50 Keywords: Physical activity, children, MVPA, ActiGraph, GENEActiv, cut-point

51 Introduction

52 Objective measures of physical activity, specifically uniaxial hip-worn 53 accelerometers, were introduced into national surveys in the US (National Health and 54 Nutrition Examination Survey, NHANES) in 2003 (29), Canada (Canada Health 55 Measures Survey) in 2007 (7,8) and the UK (Health Survey for England) in 2008 56 (17). Also in 2008, the International Children's Accelerometry Database (ICAD) was 57 initiated: a compilation of accelerometer-derived estimates of children's physical 58 activity from a wide range of studies, settings, and countries (28). The accelerometers 59 employed in these surveys and studies converted accelerations into proprietary counts 60 stored in 5-60 s epochs and time accumulated in moderate-to-vigorous physical 61 activity (MVPA) was subsequently estimated. 62 63 Over the past decade there have been rapid developments in accelerometry resulting 64 in the commercial availability of triaxial microelectromechanical (MEMS) 65 accelerometers that continuously sample and store raw accelerations at up to 100 Hz, 66 such as the ActiGraph GT3X+ and the GENEActiv. There has also been a move to 24 67 h wear protocols with wrist-wear to maximize compliance (2,9,14) and facilitate 68 measurement of the full spectrum of physical behaviours (physical activity, sedentary 69 behavior and sleep) (6). As a result, since 2011, wrist-worn ActiGraph GT3X+ 70 monitors that collect and store raw accelerations at 100 Hz have been used in 71 NHANES (30). Other large-scale adult (2,9,21) and children's (9,10,20,34) studies 72 are also employing 24 h wrist-worn accelerometer protocols using the GENEActiv. 73

As the ActiGraph GT3X+ and the GENEActiv store raw accelerations rather than
proprietary counts, their data should, theoretically, be comparable. Output from the

GENEActiv and the Actigraph GT3X+, when processed and calibrated identically
using the open source package GGIR (32,33) in R [http:/cran.r-project.org], have high
agreement for acceleration magnitudes >50-80 mg, indicative of light activity and
MVPA, although not for lower acceleration magnitudes indicative of sedentary time
(27).

81

82 Advances in measurement methods (e.g. self-report to objective measurement) and/or 83 measurement technologies (e.g. proprietary count uniaxial accelerometers to raw 84 acceleration triaxial accelerometers) bring reduced bias, improved precision and 85 enhanced measurement opportunities (30), but at a cost of limited comparability to 86 past data. There is a wealth of MVPA data on children estimated from uniaxial hip-87 worn ActiGraphs (28,29) and it is desirable to use these data to: contextualize future 88 estimates of MVPA; map trends in physical activity; compare effectiveness of past 89 and present interventions; and understand the clinical significance of intervention 90 changes in PA, by contextualizing current data with the extant historical evidence on 91 the impact of physical activity on health. To complicate comparisons further, hip-92 worn ActiGraph data have been analyzed using an extensive range of cut-points 93 leading to widely varying estimates of MVPA even for the same dataset (4,5,15).

94

95 The purpose of this study is to provide a means for quickly and simply comparing raw 96 acceleration data from wrist-worn accelerometers at a group level to past estimates of 97 children's MVPA from a range of cut-points applied to hip-worn ActiGraph data. To 98 do this, we used data from three studies that have concurrent 7-day accelerometer 99 wear at the wrist (GENEActiv) and hip (ActiGraph) to determine and cross-validate 100 the acceleration magnitudes most closely associated with established MVPA cut-

101	points. As the GENEActiv and ActiGraph GT3X+ have high agreement for
102	accelerations indicative of light activity and MVPA (27), the results will be applicable
103	to studies measuring raw triaxial accelerations at the wrist in children with either the
104	ActiGraph GT3X+ or the GENEActiv.
105	
106	Methods
107	
108	This is a secondary data analysis using data from three studies: 1) 58 children, aged
109	10-12 years, recruited from primary schools in South Australia (26); 2) 129 children,
110	aged 9-10 years, recruited from primary schools in Liverpool, UK (12); 3) 81
111	children, aged 9-11 years, recruited from one primary school in Liverpool, UK. The
112	appropriate university research ethics committee approved each study. Written
113	informed consent and assent were obtained from the parents/guardians and children,
114	respectively. Height was measured to the nearest 0.1 cm and body mass to the nearest
115	0.1 kg.
116	
117	Assessment of activity
118	
119	Free-living physical activity was measured by concurrent wear of the GENEActiv on
120	the non-dominant wrist and the ActiGraph GT3X+ positioned above the right hip, on
121	an elasticated belt worn around the waist, for seven consecutive days. In study 1,
122	children were requested to wear both monitors day and night, removing the hip-worn
123	ActiGraph for water-based activities only. In studies 2 and 3, children were requested
124	to wear both monitors at all times except when sleeping or during water-based
125	activities.

127 Accelerometers

129	The GENEActiv is a triaxial accelerometry-based activity monitor with a dynamic
130	range of +/- 8g (Gravity Estimator of Normal Everyday Activity, ActivInsights Ltd,
131	Cambridgeshire, UK). The ActiGraph GT3X+ is a triaxial accelerometry-based
132	activity monitor with a dynamic range of +/- 6 g (ActiGraph LLC, Pensacola, FL,
133	USA). Study 1: The GENEActivs were initialized to collect data at 87.5 Hz and data
134	uploaded using GENEActiv PC software version 2.2. The ActiGraphs were initialized
135	to collect data at 80 Hz and data uploaded using Actilife version 6.5.3. Data were
136	collected between April and December 2012. Studies 2 and 3: The GENEActivs and
137	ActiGraphs were both initialized to collect data at 100 Hz and data uploaded using
138	GENEActiv PC software version 2.2 and Actilife version 6.11.4, respectively. Study
139	2 data were collected between January and May 2014 and study 3 data were collected
140	in January and February 2015.
141	
142	Data processing
143	
144	Wrist-worn GENEActiv (raw acceleration) GENEActiv .bin files were analysed with
145	R-package GGIR version 1.2-0 (<u>http://cran.r-project.org</u>) (32,33). Signal processing in
146	GGIR includes the following steps: 1. Autocalibration using local gravity as a
147	reference (32); 2. Detection of sustained abnormally high values; 3. Detection of non-
148	wear; 4. Calculation of the average magnitude of dynamic acceleration, i.e. the vector
149	magnitude of acceleration corrected for gravity (Euclidean Norm minus 1 g, ENMO)
150	over user-defined s epochs:

151 ENMO = $\sum \sqrt{x^2 + y^2 + z^2} - g$ with negative values set to zero. In study 1, 152 ENMO was averaged over 5 s epochs; in studies 2 and 3, ENMO was averaged over 1 153 s epochs. As studies applying GGIR to wrist accelerometer data have used both 1 s 154 (12) and 5 s epochs (9), inclusion of both epochs increases the generalizability of the 155 findings.

156

157 Files were excluded from all analyses if post-calibration error was greater than 0.02 g158 (9) and individual days were classified as invalid and excluded if wear-time was 159 insufficient (16 h for the 24 h protocol in study 1, 10 h for the waking wear protocol 160 in studies 2 and 3). Detection of non-wear has been described in detail previously 161 (See 'Procedure for non-wear detection' in supplementary document to van Hees et 162 al. (33)). In brief, non-wear is estimated based on the standard deviation and value 163 range of each axis, calculated for 60 min windows with 15-min moving increments. If 164 for at least 2 out of the 3 axes the SD is less than 13 mg or the value range is less than 165 50 mg the time window is classified as non-wear. The default non-wear setting was 166 used, i.e. invalid data were imputed by the average at similar timepoints on different 167 days of the week

168



176	Data were	analyzed	using A	Actilife	version	6.13.0.	The raw.	gt3x f	iles were
			()					<i>(</i>)	

summarized into uniaxial (vertical) proprietary counts in 1 s, 5 s, 15 s and 60 s

178 epochs, resulting in four ActiGraph files for analysis per participant. Non-wear was

defined as 60 min of consecutive zero counts, with an allowance for 1-2 min of counts

180 between 0 and 100 (29). Individual days were classified as invalid and excluded if

181 wear-time was insufficient (16 h for the 24 h protocol in study 1, 10 h for the waking

182 wear protocol in studies 2 and 3).

183



185 (counts per minute), approximately equivalent to the cut-point for an 11 y old (3

186 METs) using the age-specific criteria of the Freedson group, published by Trost et al.

187 (31)); low (1680 cpm, Pate et al. (23)); medium (2296 cpm, Evenson et al. (11)); high

188 (3200 cpm, Puyau et al. (24)). This resulted in 16 outputs per participant: MVPA

189 classified using very low, low, medium and high cut-points, with each cut-point

applied to data integrated into 1 s, 5 s, 15 s and 60 s epochs.

191

192 Data analysis



201 epochs. The 5 s data from study 1 and the 1 s data from studies 2 and 3 were
202 designated a ≤5 s epoch.

204	Descriptive statistics (mean \pm SD) were calculated for all variables. Data from studies
205	1 and 2 (approximately 70% of the total sample) were analyzed with data from study
206	3 reserved for cross validation. The wrist-worn GENEActiv ENMO thresholds (100+,
207	150 +, 200+, 250+, 300+, 350+, 400+ mg) which most closely approximated time
208	accumulated in each of the hip-worn ActiGraph MVPA cut-points (very low, low,
209	medium, high) for each epoch length (≤ 5 s, 15 s, 60 s) were examined with a series of
210	limits of agreement (LoA) analyses (3) and intra-class correlations (ICC, single
211	measures, absolute agreement) with 95% confidence intervals (CI).
212	
213	For each hip-worn ActiGraph MVPA cut-point / epoch combination, the wrist-worn
214	ENMO threshold with the closest agreement was selected and the agreement between
215	these optimal pairings tested in the independent cross-validation sample. The
216	distributions for each of the optimal pairings were illustrated on kernel density plots
217	(bandwidth = 10) for the total sample (data from studies 1, 2 and 3 combined).
218	
219	Results
220	
221	Demographic data, by study, are presented in Table 1. The final sample size was 238
222	(Test sample $N = 159$, Cross-validation sample $N = 79$) with 30 participants excluded
223	due to no days of concurrent valid wear for both monitors. Figure 1 shows the time
224	recorded in each of the intensity categories by the hip-worn ActiGraph (very low,
225	low, medium and high MVPA cut-points) and the wrist-worn GENEActiv (100+,

226	150+, 200+, 250+, 300+, 350+, 400+ mg ENMO thresholds) by epoch (ActiGraph \leq 5
227	s, 15 s, 60 s; GENEActiv \leq 5s) for the total sample.

229 Test sample

231	The agreement between each wrist-worn GENEActiv ENMO threshold and each hip-
232	worn ActiGraph MVPA cut-point is shown for each epoch length in Table 2. The
233	ENMO threshold with the highest agreement for each ActiGraph MVPA cut-point $/$
234	epoch combination is highlighted in bold in Table 2. The optimal wrist-worn ENMO
235	thresholds for comparison to hip-worn ActiGraph MVPA cut-points were:
236	• very low MVPA ActiGraph cut-points (1100 cpm, Trost et al. (31))
237	• ENMO 150+ mg, irrespective of the ActiGraph epoch (ICC \ge 0.65,
238	mean bias (ENMO – ActiGraph) = -2.9 to -18.0 min, (-2.7 to -14.9%
239	of mean MVPA));
240	• low MVPA ActiGraph cut-points (1680 cpm, Pate et al. (23))
241	• ENMO 200+ mg, irrespective of the ActiGraph epoch (ICC \ge 0.67,
242	mean bias = -4.1 to -10.7 min (-5.4 to -13.0% of mean MVPA));
243	• medium MVPA cut-points (2296 cpm, Evenson et al. (11))
244	• ENMO 250+ mg for \leq 5 s and 15 s epochs (ICC \geq 0.69, mean bias = -
245	3.0 to -7.3 min (-5.4 to -12.0% of mean MVPA))
246	\circ ENMO 300+ mg for 60 s epochs (ICC = 0.73, mean bias = -5.0 min (-
247	10.6% of mean MVPA));
248	• high MVPA cut-points (3200 cpm, Puyau et al. (24))
249	• ENMO 300+ mg for \leq 5 s epochs (ICC = 0.73, mean bias = +1.8 min
250	(+4.7% of mean MVPA))

251	0	ENMO 350+ mg for 15 s epochs (ICC = 0.73 , mean bias = $+2.7$ min
252		(+8.7% of mean MVPA))
253	0	ENMO 400+ mg for 60 s epochs (ICC = 0.65, mean bias = $+6.5$ min
254		(+28.6% of mean MVPA)).

256 Cross-validation

257

258 The agreement of each of these optimal pairings of wrist-worn ENMO threshold and 259 hip-worn ActiGraph MVPA cut-point was tested in the cross-validation sample 260 (Table 3, Figure 2). Agreement was robust with ICC's similar to the test sample for 261 15 s epochs (very low, low and medium MVPA cut-points, mean bias = $|4.9| \pm 0.9\%$ 262 of mean MVPA) and $\approx 0.01-0.11$ lower than the test sample (0.61 to 0.71, mean bias = 263 $|8.9| \pm 4.8\%$ of mean MVPA) for other MVPA cut-point / epoch combinations, except 264 for the high MVPA cut-point / 60 s epoch where the ICC was considerably reduced 265 (0.42). The mean biases and 95% limits of agreement were also similar in magnitude 266 to the test sample. However, the values of the mean bias for specific pairings were not 267 consistent between the test sample and the cross-validation sample. 268 269 The distribution of the ActiGraph and ENMO data for each of the optimal pairings is 270 shown on kernel density plots for the total sample, Figure 3. The columns represent

271 cut-points (left to right: very low, low, medium, high) and the rows represent

ActiGraph epochs (top to bottom: ≤ 5 s, 15 s, 60 s). The agreement statistics for the

total sample are shown in Supplemental Digital Content 1.

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- 275

277

278 Discussion

280 Rapid progress in accelerometer technology has led to changes in the data collected 281 and study protocols followed, with a shift from uniaxial proprietary count outcomes 282 collected using accelerometers worn at the hip to triaxial raw accelerations measured 283 using wrist-worn accelerometers (30). We have developed a quick and simple method 284 to facilitate the comparison of group level estimates of children's MVPA from 285 uniaxial hip-worn count-based ActiGraphs to triaxial raw acceleration data measured 286 at the wrist processed using the open source R-package, GGIR (32,33). The method 287 was developed using the GENEActiv wrist-worn accelerometer, but evidence 288 suggests it will also be applicable to raw acceleration measured at the wrist using the 289 ActiGraph and processed in GGIR (27). 290

291	Mean biases for optimal pairings of ENMO thresholds and ActiGraph MVPA cut-
292	points were relatively low (test sample: mean bias = $ 9.4 \pm 4.2\%$ of mean MVPA;
293	cross-validation sample: mean bias = $ 7.8 \pm 4.9\%$ of mean MVPA) indicating good
294	group level agreement, excluding high ActiGraph MVPA cut-points assessed using a
295	60 s epoch where mean bias was high relative to the low means (29% in the test
296	sample, 60% in the cross-validation sample). Similarly, the ICC's for optimal pairings
297	were all between 0.61 and 0.76 in the test and cross-validation sample, indicating
298	good agreement (13), with the exception of the high ActiGraph MVPA cut-points
299	assessed using a 60 s epoch in the cross-validation sample (ICC = 0.42). The 95%
300	limits of agreement were moderate to large indicating that individual level

301 comparisons are not advised. The MVPA recorded in the cross-validation sample was 302 lower than the test samples, in particular when applying high cut-points with a 60 s 303 epoch (Figures 1 and 2); this may have contributed to the lower robustness for the 304 high cut-point/60 s epoch combination. Hildebrand et al. (16) developed an MVPA 305 threshold of approximately 200 mg for use with wrist-worn ActiGraph and 306 GENEActiv accelerometers. Based on the current findings, MVPA determined by 307 applying the 200 mg threshold to wrist-worn accelerometer data should compare best 308 to MVPA determined from low cut-points (23) applied to hip-worn ActiGraph data, 309 irrespective of epoch. Overall, the cross-validation suggests that agreement may be 310 closest when comparing ENMO 150+, 200+ and 250+ thresholds to MVPA estimated 311 from ActiGraph 15 s epoch data processed using very low, low and medium cut-312 points, respectively.

313

314 The potential for application of these comparisons is extensive. By 2010, over 46000 315 physical activity datasets from hip-worn ActiGraphs had been collated in the ICAD, 316 approximately 19000 from children aged 9-12 y, (28). More recently, the 317 International Study of Childhood Obesity, Lifestyle and the Environment (ISCOLE) 318 collected data on 6000 children, aged 9-11 y from 12 countries across five diverse 319 regions of the world using hip-worn ActiGraphs (18). The latter study collected 320 triaxial raw acceleration data using ActiGraph GT3X+ and has developed novel 321 analytical tools for application to the raw acceleration data, e.g. to determine sleep 322 duration (1), but as the hip was the measurement site these data have also been 323 summarized in proprietary counts and analyzed using count cut-points (19). Since 324 NHANES moved to assessing physical activity using triaxial raw acceleration data 325 measured at the wrist for the NHANES cycles 2011-2012 and 2013-2014 (30), many other large studies have also used wrist-worn accelerometers. For example, data have already been collected in: \approx 4000 children, aged 9-11 y, in the Child Health Checkpoint (Melbourne, Australia (34)); \approx 1800 girls, aged 11-14 y, in Girls Active (Leicester, UK (10)); \approx 1000 children, aged 8-11 y in the Cork Children's Lifestyle Study (Ireland (20)); and \approx 4000 children aged 7 y in the Pelotas Birth cohort (Brazil (9)). The comparisons presented will facilitate interpretation of these data in relation to past estimates of children's MVPA, e.g. from NHANES, ICAD and ISCOLE.

334 The data collated for this study came from three different sources and were collected 335 using two differing protocols. Study 1 took place in South Australia, used a 24 h wear 336 protocol and summarized the GENEActiv ENMO data in 5 s epochs. Studies 2 and 3 337 took place in the UK, used a waking time only protocol and summarized the ENMO 338 data in 1 s epochs. While the results were similar across studies and the cross-339 validation (study 3 data) showed the agreement statistics were robust, these 340 differences limit the internal validity of the study. However, the external validity is 341 enhanced, as results are applicable to ENMO data collected in 1 s and 5 s epochs 342 using either a waking or 24 h protocol. Given the outcome of interest was MVPA it is 343 not surprising that the use of a waking or 24 h protocol did not impact on the results. 344

ActiGraph epochs of ≤ 5 s, 15 s and 60 s were considered, whereas ENMO data were only summarized into ≤ 5 s epochs. The use of longer epochs in the past was due to the memory limitations of accelerometers (30). Accelerations were integrated onboard the accelerometer and stored in epochs, normally 60 s epochs, to ensure one week of data could be stored before downloading the data. Due to technological progress onboard memory is no longer a problem and raw acceleration data collected at 100 Hz 351 can be stored for one week. Therefore it is unlikely that epochs longer than the default 352 5 s epoch in GGIR will be used, particularly when assessing children's activity where 353 the typical sporadic activity patterns are best captured using short epochs (22). It 354 should be noted that the participants in this study were from a relatively narrow age 355 range and the results cannot be generalized beyond the 9-12 y age group tested. 356 In summary, this study indicates that, in 9-12 y old children, time accumulated above 357 358 the appropriate incremental ENMO threshold has good agreement at a group level 359 with a range of widely used very low to high ActiGraph MVPA cut-points. It is 360 important to note this is a simple pooled-data comparison study that enables group 361 level comparisons, but individual level comparisons are not advised. We recommend 362 that when processing triaxial raw acceleration wrist accelerometer data using GGIR, 363 the times accumulated above ENMO thresholds ranging from >100 to >400 mg, or in 364 incremental acceleration bins (e.g. 9), are presented. As well as providing an activity 365 profile, this will enable the reader to quickly and simply compare the findings to past 366 estimates of children's MVPA from hip-worn ActiGraph data across a range of 367 widely used cut-points.

368

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497 Figure legends

498 Figure 1. Time recorded above each of the intensity thresholds by the hip-worn

499 ActiGraph (very low, low, medium and high MVPA count cut-points) and the wrist-

- 500 worn GENEActiv (100+, 150+, 200+, 250+, 300+, 350+, 400+ mg ENMO
- 501 thresholds) by epoch (ActiGraph ≤ 5 s, 15 s, 60 s; GENEActiv ≤ 5 s) for the total
- 502 sample. Boxplot shows the median (dark line), 25th and 75th percentiles (box), lowest
- and highest values within 1.5 times the inter-quartile range (whiskers) and outliers
- 504 (circles).

505

506 Figure 2. The time recorded above each of the intensity thresholds by the hip-worn

507 ActiGraph (very low (a), low (b), medium (c) and high (d) MVPA count cut-points)

and the wrist-worn GENEActiv acceleration threshold by epoch (ActiGraph ≤ 5 s, 15

509 s, 60 s; GENEActiv \leq 5s) for each of the optimal pairings in the cross-validation

510 sample. Boxplots show the median (dark line), 25th and 75th percentiles (box), lowest

and highest values within 1.5 times the inter-quartile range (whiskers) and outliers(circles).

513

Figure 3. Kernel density plots showing the distribution of time recorded above each of the intensity thresholds by the hip-worn ActiGraph and the wrist-worn GENEActiv for each of the optimal pairings (total sample). The columns represent cut-points (left to right: very low, low, medium, high) and the rows represent ActiGraph epochs (top to bottom: \leq 5 s, 15 s, 60 s)

519

520 List of Supplemental Digital Content

521 Supplemental Digital Content 1. Docx

Study	Valid N	Age (y)	Height (cm)	Mass (kg)
	(boys)			
1	51 (26)	11.3 ± 0.6	148.7 ± 6.8	44.1 ± 11.2
2	108 (42)	10.0 ± 0.3	139.1 ± 7.6	35.4 ± 8.5
1 & 2 (Test sample)	159 (68)	10.4 ± 0.7	142.2 ± 8.6	38.3 ± 10.3
3 (Cross-validation sample)	79 (5)	10.3 ± 0.6	142.1 ± 7.8	36.9 ± 8.6
Total sample	238 (103)	10.4 ± 0.7	142.2 ± 8.3	37.8 ± 9.7

522 Table 1. Participant characteristics (mean \pm standard deviation (SD))

Table 2. Agreement between each hip-worn ActiGraph cut-point and each wrist-worn GENEActiv ENMO threshold by epoch length in the test sample
 (N=159)

HIP	WRIST	ActiGraph ≤5 s epoch			Acti	Graph 15 s epoc	h	ActiGraph 60 s epoch			
ActiGraph cut-point	GENEActiv ENMO ^e (mg)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	
Very low ^a	100+	0.29	55.9	59.6	0.43 (-0.10, 0.72)	42.8	58.7	0.47 (-0.08, 0.75)	40.7	61.6	
	150+	0.71 (0.62, 0.78)	-2.9	43.9	0.67 (0.33, 0.82)	-15.9	44.1	0.65 (0.31, 0.81)	-18.0	49.5	
	200+	0.36	-34.6	39.6	0.30	-47.7	41.8	0.31	-49.8	49.4	
	250+	0.18	-53.0	39.4	0.16	-66.0	43.4	0.18	-68.1	52.2	
	300+	0.11	-64.3	40.0	0.10	-77.3	45.3	0.12	-79.4	54.9	
	350+	(0.08) (-0.03) (0.28)	-71.8	40.8	0.08	-84.9	47.1	0.09	-87.0	57.1	
	400+	0.06	-77.2	41.7	0.06	-90.3	48.7	0.07	-92.4	59.0	
Low ^b	100+	0.16 (-0.06, 0.44)	80.4	61.6	0.18 (-0.06, 0.49)	79.8	60.9	0.17 (-0.06, 0.47)	86.4	63.0	
	150+	0.53 (0.01, 0.77)	21.6	41.2	0.59 (0.05, 0.81)	21.0	40.6	0.53 (-0.07, 0.79)	27.6	42.7	
	200+	0.67 (0.41, 0.80)	-10.1	32.7	0.71 (0.44, 0.83)	-10.7	33.5	0.75 (0.67, 0.81)	-4.1	36.4	
	250+	0.37 (-0.09, 0.70)	-28.5	30.1	0.41 (-0.10, 0.73)	-29.1	32.5	0.51 (-0.06, 0.77)	-22.5	36.1	
	300+	0.22 (-0.06, 0.55)	-39.8	29.6	0.25 (-0.07, 0.59)	-40.4	33.3	0.33 (-0.10, 0.66)	-33.8	37.5	
	350+	0.15 (-0.04, 0.44)	-47.3	29.9	0.18 (-0.06, 0.49)	-47.9	34.5	0.23 (-0.08, 0.56)	-41.3	39.0	

	400+	0.11	-52.7	30.6	0.13	-53.3	35.9	0.18	-46.7	40.5
		(-0.04, 0.36)			(-0.05, 0.41)			(-0.07, 0.47)		
Medium ^c	100 +	0.09	101.6	65.9	0.09	105.8	65.5	0.08	115.2	66.9
	1.50	(-0.04, 0.29)	10 0	10.1	(-0.04, 0.31)		10.0	(-0.04, 0.28)		10.0
	150+	0.26	42.8	43.1	0.27	47.1	42.2	0.21	56.4	43.3
		(-0.09, 0.59)			(-0.08, 0.60)			(-0.06, 0.54)		
	200+	0.63	11.1	31.7	0.61	15.3	31.1	0.48	24.7	32.0
		(0.30, 0.79)			(0.09, 0.82)			(-0.10, 0.77)		
	250+	0.69	-7.3	26.4	0.76	-3.0	26.7	0.73	6.4	27.7
		(0.48, 0.80)			(0.69, 0.82)			(0.59, 0.82)		
	300+	0.46	-18.6	24.3	0.58	-14.4	25.6	0.73	-5.0	26.6
		(-0.10, 0.76)			(0.00, 0.81)			(0.61, 0.81)		
	350+	0.30	-26.1	23.6	0.41	-21.9	25.7	0.58	-12.5	26.9
		(-0.08, 0.65)			(-0.10, 0.73)			(0.10, 0.79)		
	400+	0.22	-31.5	23.6	0.30	-27.3	26.4	0.45	-17.9	27.6
		(-0.06, 0.55)			(-0.08, 0.64)			(-0.08, 0.73)		
High ^d	100+	0.05	122.0	71.3	0.04	130.4	72.1	0.03	139.5	73.9
111811	1001	(-0.03, 0.17)	12210	, 110	(-0.03, 0.16)	10001	,	(-0.02, 0.13)	10,10	1017
	150 +	0.12	63.3	47.1	0.10	71.7	47.8	0.07	80.7	49.6
		(-0.05, 0.37)			(-0.05, 0.33)			(-0.04, 0.27)		
	200+	0.28	31.6	33.4	0.21	40.0	34.1	0.15	49.0	35.6
		(-0.09, 0.61)			(-0.07, 0.54)			(-0.05, 0.43)		
	250+	0.54	13.2	25.7	0.40	21.6	27.3	0.26	30.7	27.6
		(0.03, 0.77)			(-0.10, 0.71)			(-0.08, 0.59)		
	300+	0.73	1.8	21.5	0.60	10.3	22.3	0.40	19.3	23.2
		(0.65, 0.80)			(0.12, 0.80)			(-0.10, 0.71)		
	350+	0.69	-5.7	19.3	0.73	2.7	20.2	0.54	11.8	20.8
		(0.46, 0.81)			(0.64, 0.80)		_	(-0.02, 0.78)		
	400+	0.55	-11.1	18.3	0.72	-2.6	19.2	0.65	6.5	19.5
	1001	(-0.04, 0.80)		10.0	(0.64, 0.80)	2.0	17.2	(0.36, 0.79)	0.2	17.0
		(0.04, 0.00)			(0.07, 0.00)			(0.00, 0.77)		

= 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31)= 1680 cpm, Pate et al. (23)526 ^aVery low 527 ^bLow

- 528 ^cMedium = 2296 cpm, Evenson et al. (11)
- 529 ^dHigh = 3200 cpm, Puyau et al. (24)
- 530 ^eENMO = Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity
- 531 ^fICC = Intra-class correlation coefficient
- 532 $^{g}95\%$ CI = 95% confidence interval
- 533 ^hLoA = Limits of agreement
- 534 The ENMO threshold with the highest agreement for each ActiGraph count cut-point / epoch combination is highlighted in bold.
- 535

	GENEActiv	Act	iGraph <u><</u> 5 s epo	ch	ActiGr	aph 15 s epoch		ActiGra	aph 60 s epoc	h
ActiGraph cut-point HIP	ENMO ^e (mg) WRIST	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)
Very low ^a	150+	0.63 (0.46, 0.75)	7.0	39.4	0.71 (0.57, 0.80)	-5.9	39.1	0.69 (0.55, 0.80)	-6.2	42.6
Low ^b	200+	0.66 (0.51, 0.77)	-3.8	31.0	0.71 (0.58, 0.80)	-3.0	31.2	0.69 (0.55, 0.80)	5.3	32.8
Medium ^c	250+	0.64 (0.49, 0.76)	-3.6	25.7	0.70 (0.57, 0.80)	2.0	13.1			
	300+							0.69 (0.56, 0.79)	2.2	23.8
High ^d	300+	0.62 (0.46, 0.74)	2.7	21.5						
	350+				0.61 (0.33, 0.76)	5.5	18.7			
	400+							0.42 (-0.04, 0.69)	9.7	18.2

Table 3. Cross-validation sample: Agreement between the hip-worn ActiGraph and wrist-worn GENEActiv for the optimal ENMO threshold for each ActiGraph count cut-point / epoch combination (N = 79)

538

³Very low = 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31)

540 ^bLow = 1680 cpm, Pate et al. (23)

541 °Medium = 2296 cpm, Evenson et al. (11)

542 ^dHigh = 3200 cpm, Puyau et al. (24)

543 ^eENMO = Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity

544 ^fICC = Intra-class correlation coefficient

545 g95% CI = 95% confidence interval

546 ^{h}LoA = Limits of agreement

548 Supplementary Table. Agreement between each hip-worn ActiGraph cut-point and each wrist-worn GENEActiv ENMO threshold by epoch length in

549 the total sample (N = 238)

HIP	WRIST	Act	iGraph <u><</u> 5 s epoc	ch	ActiGr	caph 15 s epoch		ActiGra	ph 60 s epoch	
ActiGraph cut-point	GENEActiv ENMO ^e (mg)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)
Very low ^a	100+	0.27 (-0.09, 0.60)	57.5	59.6	0.36 (-0.10, 0.68)	44.5	57.1	0.44 (-0.09, 0.73)	43.0	59.6
	150+	0.70 (0.63, 0.76)	0.4	43.4	0.68 (0.57, 0.76)	-12.6	43.4	0.67 (0.45, 0.79)	-14.1	48.5
	200+	0.39	-30.5	38.6	0.34	-43.5	40.9	0.33	-45.0	48.0
	250+	0.19	-48.4	38.0	0.18	-61.4	42.2	0.18	-62.9	50.4
	300+	0.12	-59.4	38.5	0.12	-72.4	44.0	0.12	-73.9	52.8
	350+	(-0.04, 0.39) 0.09	-66.8	39.3	(-0.05, 0.37) 0.08	-79.8	45.7	(-0.05, 0.37) 0.09	-81.3	54.8
	400+	(-0.04, 0.29) 0.064 (-0.03, 0.24)	-72.0	40.2	(-0.04, 0.29) 0.07 (-0.04, 0.24)	-85.0	47.3	(-0.04, 0.30) 0.07 (-0.04, 0.25)	-86.5	56.6
Low ^b	100+	0.15	79.9	80.0	0.16 (-0.06, 0.46)	79.9	59.5	0.16 (-0.05, 0.45)	87.1	61.1
	150+	0.50 (-0.02, 0.75)	22.9	41.1	0.54 (-0.01, 0.78)	22.8	40.5	0.48 (-0.09, 0.76)	29.9	42.6
	200+	0.68 (0.51, 0.78)	-8.0	32.7	0.71 (0.54, 0.80)	-8.2	33.4	0.74 (0.68, 0.80)	-1.0	36.3
	250+	0.39	-25.9	29.7	0.42	-26.0	32.1	0.54 (0.01, 0.77)	-18.9	35.6
	300+	0.23	-36.9	29.0	0.25	-37.1	32.6	0.35	-29.9	36.6
	350+	0.15 (-0.05, 0.45)	-44.3	29.2	0.18 (-0.06, 0.48)	-44.4	33.7	0.25 (-0.09, 0.57)	-37.3	37.9

	400+	0.11	-49.5	29.7	0.13	-49.7	34.9	0.19	-42.5	39.3
		(-0.04, 0.37)			(-0.05, 0.40)			(-0.08, 0.49)		
Medium ^c	100+	0.08	99.9	66.1	0.08	104.6	64.0	0.07	114.4	65.5
		(-0.04, 0.28)			(-0.04, 0.29)			(-0.03, 0.26)		
	150 +	0.25	42.8	42.9	0.25	47.4	42.1	0.19	57.3	43.4
		(-0.09, 0.57)			(-0.08, 0.58)			(-0.06, 0.51)		
	200 +	0.60	11.8	31.7	0.59	16.5	33.4	0.43	26.3	32.5
		(0.25, 0.77)			(0.10, 0.79)			(-0.10, 0.74)		
	250+	0.68	-6.1	26.4	0.74	-1.4	26.7	0.69	8.5	27.9
		(0.53, 0.78)			(0.67, 0.79)			(0.45, 0.81)		
	300+	0.47	-17.1	24.0	0.55	-12.4	25.3	0.73	-2.6	26.5
		(-0.09, 0.75)			(-0.02, 0.79)			(0.66, 0.78)		
	350+	0.31	-24.5	23.2	0.38	-19.8	25.2	0.61	-9.9	26.5
		(-0.08, 0.65)			(0.10, 0.71)			(0.25, 0.78)		
	400 +	0.22	-29.7	23.1	0.28	-24.9	25.7	0.48	-15.2	27.0
		(-0.06, 0.55)			(-0.08, 0.61)			(-0.03, 0.73)		
High ^d	100 +	0.04	119.1	71.4	0.04	128.0	70.5	0.03	137.1	72.7
0		(-0.03, 0.17)			(-0.03, 0.15)			(-0.02, 0.12)		
	150 +	0.11	62.0	46.5	0.10	70.9	47.3	0.07	79.9	49.5
		(-0.05, 0.36)			(-0.05, 0.31)			(-0.04, 0.24)		
	200 +	0.26	31.1	33.3	0.21	39.9	33.4	0.13	49.0	36.0
		(-0.09, 0.58)			(-0.08, 0.52)			(-0.05, 0.40)		
	250 +	0.51	13.2	25.7	0.40	22.1	26.3	0.23	31.1	28.0
		(0.02, 0.75)			(-0.09, 0.69)			(-0.08, 0.55)		
	300+	0.71	2.1	21.5	0.60	11.0	22.1	0.35	20.1	23.4
		(0.64, 0.77)			(0.30, 0.76)			(-0.10, 0.67)		
	350+	0.68	-5.2	19.2	0.70	3.7	19.9	0.48	12.7	20.8
		(0.48, 0.79)			(0.63, 0.76)			(-0.06, 0.75)		
	400 +	0.54	-10.5	18.1	0.65	-1.6	18.7	0.59	7.5	19.3
		(-0.03, 0.78)			(0.48, 0.76)			(0.22, 0.36)		
	350+ 400+	(0.64, 0.77) 0.68 $(0.48, 0.79)$ 0.54 $(-0.03, 0.78)$	-5.2 -10.5	19.2 18.1	(0.50, 0.76) 0.70 (0.63, 0.76) 0.65 (0.48, 0.76)	3.7 -1.6	19.9 18.7	(-0.10, 0.87) 0.48 (-0.06, 0.75) 0.59 (0.22, 0.36)	12.7 7.5	

= 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31)= 1680 cpm, Pate et al. (23)550 551 ^aVery low ^bLow

- 552 "Medium = 2296 cpm, Evenson et al. (11)
- 553 ^dHigh = 3200 cpm, Puyau et al. (24)
- ⁶ENMO = Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity
- 555 ^fICC = Intra-class correlation coefficient
- 556 ^g95% CI = 95% confidence interval
- 557 ^hLoA = Limits of agreement
- 558 The ENMO threshold with the highest agreement for each ActiGraph count cut-point / epoch combination in the test sample is highlighted in bold.
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