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1 **PHYSIOTHERAPY - AGE-RELATED CHANGES IN PHYSICAL FUNCTIONING: CORRELATES**  
2 **BETWEEN OBJECTIVE AND SELF-REPORTED OUTCOMES**

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10  
11 **ABSTRACT**

12 **Objectives:** Firstly, to quantify the variance attributable to age and estimate annual decline in  
13 physical function and self-reported health using a battery of outcome measures in healthy older  
14 females. Secondly, to determine whether self-reported functional losses are similar to those  
15 measured objectively and which best represent overall physical capacity.

16 **Design:** Experimental study, cross-sectional analysis.

17 **Setting:** Human Performance Laboratory, University setting.

18 **Participants:** Thirty-nine community-dwelling women (Mean[SD] age=71.5[7.3]years, range 60-  
19 83years) completed a battery of *objective* measures of function and a *self-reported* health status  
20 survey.

21 **Intervention:** None.

22 **Main outcome measures:** *Objective measures:* Gait speed; TUG test; sit-to-stand; concentric  
23 knee flexor and extensor moments; *self-reported:* the SF-36.

24 **Results:** Using a cross-sectional approach, annual declines were estimated for: TUG time (2.1%);  
25 gait speed (1.2%); knee extensor (2.2%) and flexor moments (3.0%); and *self-reported* Physical  
26 Functioning (0.9-1.2%) ( $p \leq .001$ ). Linear regression indicated that age explained moderate variance  
27 in the *objective* ( $R^2=21-34\%$ ) and *self-reported* ( $R^2=14-28\%$ ) outcomes. TUG time and gait speed  
28 was significantly correlated with all *objective* outcomes except sit-to-stand ( $r=0.46-0.83$ ) and most  
29 of the *self-reported* ( $r=0.10-0.63$ ) outcomes ( $p < .01$ ).

30 **Conclusions:** Age-related functional deterioration was estimated precisely across both objective  
31 and self-reported outcomes. Greater strength losses for the knee flexors compared to the  
32 extensors indicate an unequal strength loss of antagonistic muscle pairs which has implications for  
33 the safe completion of many functional tasks including obstacle negotiation, stair locomotion,  
34 postural transitions, and ultimately knee joint stability. Furthermore, walking speed and TUG time  
35 correlated most strongly with many of the outcomes highlighting their importance as global  
36 indicators of physical capacity.

37

38 **Keywords:** healthy ageing; objective and self-reported outcomes; physical capacity; functional  
39 performance

40

## 41 INTRODUCTION

42 The ability to perform common activities of daily living (ADL) autonomously is essential for  
43 independence and mobility. However, as we age, a combination of physical and psychological  
44 changes reduces our ability to complete these daily tasks(1-6). This may lead to increased  
45 sedentary behaviour, task avoidance and ultimately poorer quality of life(7). Government statistics  
46 have confirmed that adults  $\geq 65$  years have an increased life expectancy(8). Therefore, monitoring  
47 physical function within healthy older populations is critical to facilitate the early identification of  
48 decline and offer insight into the age-related loss of physical function and general health.  
49 Accordingly, the Chartered Society of Physiotherapy (CSP) has recommended that normative data  
50 for healthy older adults should be documented regularly as it provides a baseline from which age-  
51 related dysfunction may be identified(9). Furthermore, the Australian Physiotherapy Association  
52 have suggested that continued documentation is vital for monitoring, evaluating and justifying  
53 patient care(10).

54

55 An individual's ability to perform ADL can be monitored using a range of measured and self-  
56 reported outcomes(2, 3, 11). These assessments are often simple to perform, are appropriate for  
57 use with older adults(12) and individuals at risk of falling(13). Consequently, such "outcome

58 measures” are routinely used in physiotherapy, rehabilitation, occupational and geriatric  
59 settings(14) where they provide information about functional mobility(15), prospective falls risk(16),  
60 and offer moderate-to-good test-retest reliability(16, 17). Objectively measured functional losses  
61 (gait speed, chair-stand time, grip strength, and balance) correlate moderately with self-reported  
62 functioning (r ranged from -.19 to-.63,  $p<.05$ )(18), and gait speed appears to be a global indicator  
63 of function over a broad range of capacities(18). Selecting the most appropriate battery of  
64 outcomes can be challenging for health professionals and is often dependent on the population of  
65 interest, the nature of the visit (i.e., routine check-up, hospital admission), and the  
66 equipment/expertise available.

67

68 Existing evidence originating from segmented age-group comparisons (ie. according to decade 60-  
69 69y, 70-79y etc) suggests that physical function worsens as older age ensues and that the decline  
70 is linear(2, 3, 5, 6), but the year-on-year progression of this deterioration is less defined. For  
71 example, the time taken to complete the ‘Timed get-Up and Go’ (TUG) test increases by ~40%  
72 (8.1–11.3s) between the ages of 60-99years(3) but the annual rate at which declines occur is less  
73 clear. Similar limitations in our knowledge exist with regards to the sit-to-stand (STS) task(4, 5).  
74 Comfortable gait speeds gradually slow with advancing age(19), and grouped means suggest that  
75 greater declines occur >79years(1). Lower limb strength decreases continuously across intervals  
76 of older age(20) with a 19% loss in knee extensor strength reportedly occurring across the 8<sup>th</sup>  
77 decade(21). Age-related changes in the SF-36 sub-scales indicate that, in general, the physical  
78 components deteriorate while the mental components remain constant or show small increases  
79 across age-grouped samples(22). However, these data do not include adults aged over 64 years,  
80 thus restricting generalisations to older populations. Very few studies have attempted to quantify  
81 annual losses in physical function, meaning subtle yet important changes may be overlooked when  
82 age-related decline is generalised from wide pre-defined sub-divisions of old age. Moreover,  
83 evaluating functional changes across broad age ranges makes it difficult to monitor functional  
84 decline across a shorter period of time and may mean that the optimal time to intervene could be  
85 missed inadvertently.

86

87 The few previous studies that have quantified annual changes have solely focused on the age-  
88 related change in functional performance in isolation such as muscle strength(21, 23), balance(24),  
89 measures of walking speed(25), and self-reported physical function only without substantiating  
90 objective measures(26). Moreover, TUG time has been used to estimate changes in a single(14) or  
91 a battery of outcomes (comfortable and fast gait speed, balance, TUG, STS, 6-minute walk time,  
92 and physical performance test)(1). Whilst the authors presented a range of measures, the study  
93 used both age and the use of an assistive device to understand age-related decline(1).  
94 Understanding the subtle nature of these losses that occur across the older age spectrum in a  
95 battery of outcomes will guide timely intervention to attenuate functional decline.

96

97 The aims of this study were to: (i) quantify annual changes in physical function in a convenience  
98 sample of healthy, older community-dwelling women across a battery of clinical outcomes; and (ii)  
99 to determine whether self-reported functional losses are similar to those measured objectively and  
100 which outcomes best represent overall physical capacity. It was hypothesised that linear  
101 relationships would exist between physical function and age with minimal annual (year-on-year)  
102 changes expected in self-reported well-being, throughout the age spectrum.

103

## 104 **METHODS**

### 105 **PARTICIPANTS**

106 Thirty-nine healthy, community-dwelling older women (Mean age[SD] 71.5[7.3] years, height  
107 1.63[0.07]m, mass 70.6[12.4]kg) with no prior falls history gave written consent to participate in this  
108 study which was approved by the local NHS Ethics Committee (08/H1305/91). This work forms  
109 part of a larger set of studies that evaluated the influence of healthy ageing on the biomechanical  
110 profiles of ADL (27, 28). Due to technical failure during data acquisition, missing data were  
111 recorded for the STS test (n=37 remaining) and knee dynamometry (n=35 remaining).

112

113 **OUTCOME MEASURES**

114 The TUG and the STS tasks were assessed using the same standard chair with no arm rests (seat  
115 height:46cm, depth:38cm, and back height:74cm)(14, 15). A standard TUG test protocol was  
116 employed(29) whereby participants began seated, stood up, walked to and around a cone 3-  
117 metres away, and returned to a seated position. Participants were asked to complete the  
118 movement as quickly and safely as possible, refraining from using their arms for assistance during  
119 the chair rise, thus relying predominantly on the lower limbs for task completion. The movement  
120 was performed three times and the time to complete each trial was recorded using a stopwatch. To  
121 assess STS performance, participants began seated, and when ready stood up at their  
122 comfortable speed. Sagittal plane kinematics were measured at 100Hz (Qualisys, Sweden) to  
123 determine the time taken to complete one STS cycle. Movement initiation was defined as an  
124 increase in hip flexion of >1% of the maximum hip flexion during the movement (exhibited as  
125 increased forward trunk lean) that was shortly followed by knee extension. Maximum knee  
126 extension determined movement termination. Gait speed was derived from gait analysis data  
127 reported previously for the same sample(27). Briefly, 8-10 trials were collected while participants  
128 walked along a 10-metre walkway at a comfortable pace. Steady-state gait speed was obtained  
129 from the central part of the walkway and averaged across trials.

130

131 Knee flexor and extensor concentric strength were assessed bilaterally using dynamometry across  
132 the participants' full range of knee motion while the hip was flexed at 90° (Biodex System 3, Biodex  
133 Medical, Shirley, NY). Straps were secured around the trunk and hips for stability. The knee axis of  
134 rotation was aligned with the dynamometer axis of rotation and the dynamometer lever arm was  
135 secured to the distal end of the shank. Five practise trials were performed. Gravity corrected joint  
136 moments were recorded while participants performed maximal voluntary concentric contractions  
137 during five consecutive knee extension-flexion trials. Verbal encouragement was provided  
138 throughout. The angular speed of 180°/sec has been used previously with older adults(20) and  
139 concentric exercises have been shown to elicit significantly less cardiovascular stress than  
140 eccentric testing(30). Therefore, concentric testing at a high angular speed was chosen to

141 minimise cardiovascular stress and avoid potential injury(31). The SF-36 is regarded as a generic  
142 measure of health status(17). The survey is comprised of 36 questions covering both physical and  
143 mental health, each of which is composed of 4 sub-scales. Administration of each test was  
144 standardised to the following order: TUG test, STS, knee strength, gait speed and SF-36, as the  
145 first two assessments served as a whole body warm-up prior to strength testing.

146

## 147 **DATA ANALYSIS**

148 The fastest TUG time from the three trials obtained was selected for further analysis(32) permitting  
149 task familiarisation. The time taken to complete a single STS cycle comfortably was used. Knee  
150 moments were normalised to body weight (Nm/kg). The hamstrings-to-quadriceps (H:Q) ratio was  
151 calculated from the peak joint moments. Paired-samples t-tests indicated that no significant  
152 strength differences existed between the right and left limbs so were combined for all analyses.

153

154 The SF-36 was analysed according to the 8 sub-scales: Physical Functioning, Role limitations due  
155 to physical health problems (Role–Physical), Bodily Pain, General Health, Vitality, Social  
156 Functioning, Role limitations due to emotional problems (Role–Emotional), and Mental Health(33).  
157 In the event of missing data, scores were estimated per participant by averaging the answers given  
158 within the section of questions with missing data(33). Of the 1404 questions (36 questions, 39  
159 participants) only 30 data points were missing for nine participants. For seven participants, missing  
160 data were estimated and two participants were excluded from further analysis (n=37 remaining).  
161 Linear transformations were computed to transform SF-36 scores into z-scores using the norm-  
162 based scoring procedure according to the currently available normative database of the 1998  
163 general US population(34). Each of the sub-scales was aggregated using a T-score transformation  
164 to produce a Mental Component Summary (MCS) and a Physical Component Summary (PCS).

165

166 Each of the outcome measures presented were chosen for their reliability and suitability for use  
167 with older adults. Intra-class correlation coefficients(ICC) indicate how consistent or reproducible

168 a quantitative measurement is. For example, the TUG time offers high reproducibility with an ICC  
169 of 0.8 from a cohort of older people(35) and similar levels of consistency has been confirmed for  
170 STS(6). Mechanical reliability of the dynamometer is high(ICC=0.99) as is test re-test reliability of  
171 strength in older adults(ICC>0.92)(36). Respectable ICCs have also been presented for the gait  
172 speed of older adults(ICC=0.74)(5) and across the age continuum incorporating both young and  
173 old(ICC=~0.9)(2). Finally, the SF-36 is suitable for use with older populations and demonstrates  
174 good construct validity with Cronbach's alpha statistics ranging from 0.82 to 0.94 for each of the  
175 subscales(17).

176

## 177 **STATISTICAL ANALYSIS**

### 178 *Aim 1 – Estimation of annual changes in health and physical function*

179 Bivariate correlations (Pearson's r) expressed the strength of the relationship between each of the  
180 outcomes and age. Linear regression was computed for all outcomes using age as a single  
181 independent predictor. Dependent variables were plotted against age to check for linearity and  
182 statistical assumptions surrounding regressive procedures were confirmed. Outliers were  
183 determined from the standardised residuals and data  $\pm 3SD$  from the mean were considered to be  
184 extreme and unlikely to have occurred by chance therefore they were removed(37, 38). For  
185 completeness, models excluding outliers are presented within the table and models with outliers  
186 included are presented within the footnotes of the table.  $R^2$  (%) and the standardised regression  
187 coefficient (beta) are presented. Using the 75<sup>th</sup> percentile as a starting value, the annual change in  
188 function was calculated. 95% confidence intervals (95%CI) assessed the variation in estimated  
189 annual change.

190

### 191 *Aim 2 – Changes in objective and self-reported physical function*

192 Additional bivariate correlations were calculated between each of the objective and self-reported  
193 outcomes. Significance was accepted when  $p \leq .05$ .



194 **RESULTS**

195 *Aim 1 - Estimation of annual changes in health and physical function*

196 Five of the participants (aged 75, 78, 80 and two 83year olds) were unable to achieve the constant  
197 target velocity of 180°/s during the knee flexion dynamometry, and thus data for these individuals  
198 were removed from further analysis of flexion moments and H:Q ratio only. All of the objective  
199 assessments, with the exception of the STS, were significantly correlated with age ( $p \leq .01$ , Table  
200 1, Figure 1). All significant relationships, except for TUG time, were negatively correlated with age  
201 ( $r = -.46 - -.58, p \leq .05$ ). Strong negative correlations existed between age and knee strength  
202 measures (peak moments and H:Q ratio) and gait speed ( $r = -.46 - -.58, p \leq .05$ ). The strongest  
203 negative correlations were found between age and knee moments ( $r = -.58, p \leq .01$ ). Only the  
204 Physical Functioning sub-scale and PCS of the SF-36 were correlated with age ( $r = -.53$  and  $-.38$ ,  
205 respectively, Figure 2). Age contributed to explaining moderate-to-good levels of variance in all  
206 objective outcomes, except for STS time ( $R^2 = 21-34\%$ , Table 1). Significant point estimates (B)  
207 were found for all of the objective outcomes, except for STS, revealing annual changes of 1.2-  
208 3.0%/year. Age explained the greatest variance in the knee extensor ( $R^2 = 33\%$ ) and flexor  
209 ( $R^2 = 34\%$ ) moments.

210

211 Age contributed to explaining moderate-to-good levels of variance in the Physical Functioning sub-  
212 scale and PCS ( $R^2 = 28\%$  and  $14\%$ , respectively) with self-reported losses of 1.2%/year and  
213 0.9%/year, respectively. Knee flexor moments exhibited the greatest decline (3.0%/year), although  
214 95%CI were wider for the knee strength measures compared to self-rated Physical Functioning  
215 ( $\pm 1.3\%$ ) and the PCS ( $\pm 1.5\%$ ). Regression analysis could not be computed with a number of SF-36  
216 subscales, as the majority of the sample attained the maximum score (100) demonstrating that a  
217 ceiling effect had occurred: Role-Physical and Social Functioning (both  $n = 29, 74\%$  of the sample)  
218 and Role-Emotional ( $n = 32, 82\%$  of the sample).

219

220 **TABLE 1** Regression models developed to explain the variance in the outcome measures explained by advancing age

		MEAN (SD)	Correlation with Age (r)	R <sup>2</sup> (%)	REGRESSION COEFFICIENT		95% CI	ANNUAL CHANGE (%/year)	95% CI ANNUAL CHANGE
					beta	Sig.			
FUNCTIONAL MEASURES	TUG time (s) [1]	7.85 (2.9)	.53	28%	.181	p = .001	.084 : .277	+2.1%	1.0 : 3.3%
	STS time (s)	1.46 (0.26)	.15	0%	-.085	.386			
	Gait speed (m/s)	1.28 (0.20)	-.57	32%	-.017	p ≤ .001	-.026 : -.009	-1.2%	-1.9 : -0.6%
	HQ Ratio (%)	0.40 (0.15)	-.46	21%	-.010	p ≤ .001	-.017 : -.003	-2.0%	-3.4 : -0.6%
	Peak Knee Extensor Moment (Nm/kg)	0.48 (0.18)	-.58	33%	-.014	p ≤ .001	-.021 : -.007	-2.2%	-3.5 : -1.0%
	Peak Knee Flexor Moment (Nm/kg)	0.21 (0.11)	-.58	34%	-.009	p ≤ .001	-.014 : -.004	-3.0%	-4.7 : -1.3%
SELF-REPORTED MEASURES	SF36: Physical Functioning	81.7 (15.5)	-.53	28%	-1.143	p ≤ .001	-1.762 : -.525	-1.2%	-1.9 : -0.6%
	SF36: Role- Physical	84.2 (31.0)	-.19	^	^	^			
	SF36: Bodily Pain	77.4 (17.4)	-.30	9%	-.835	.065			
	SF36: General Health	73.4 (15.8)	-.21	10%	-.685	.059			
	SF36: Vitality	70.1 (16.9)	-.29	9%	-.770	.074			
	SF36: Social Functioning	93.8 (12.9)	-.03	^	^	^			
	SF36: Role – Emotional	92.1 (21.1)	-.11	^	^	^			
	SF36: Mental Health [2]	84.1 (10.3)	-.06	0%	-.105	.701			
	SF36: Mental Component Summary [3]	56.6 (5.1)	.01	0%	.008	.958			
	SF36: Physical Component Summary	50.3 (8.5)	-.38	14%	-.443	.022	-.801 : -.065	-0.9%	-1.6 : -0.1%

221 ^ indicates variables where regression could not be computed due to ceiling effects, CI denotes confidence interval, HQ: Hamstrings-to-Quadriceps Ratio.

222

223 Footnotes indicate the models with outliers included within the model

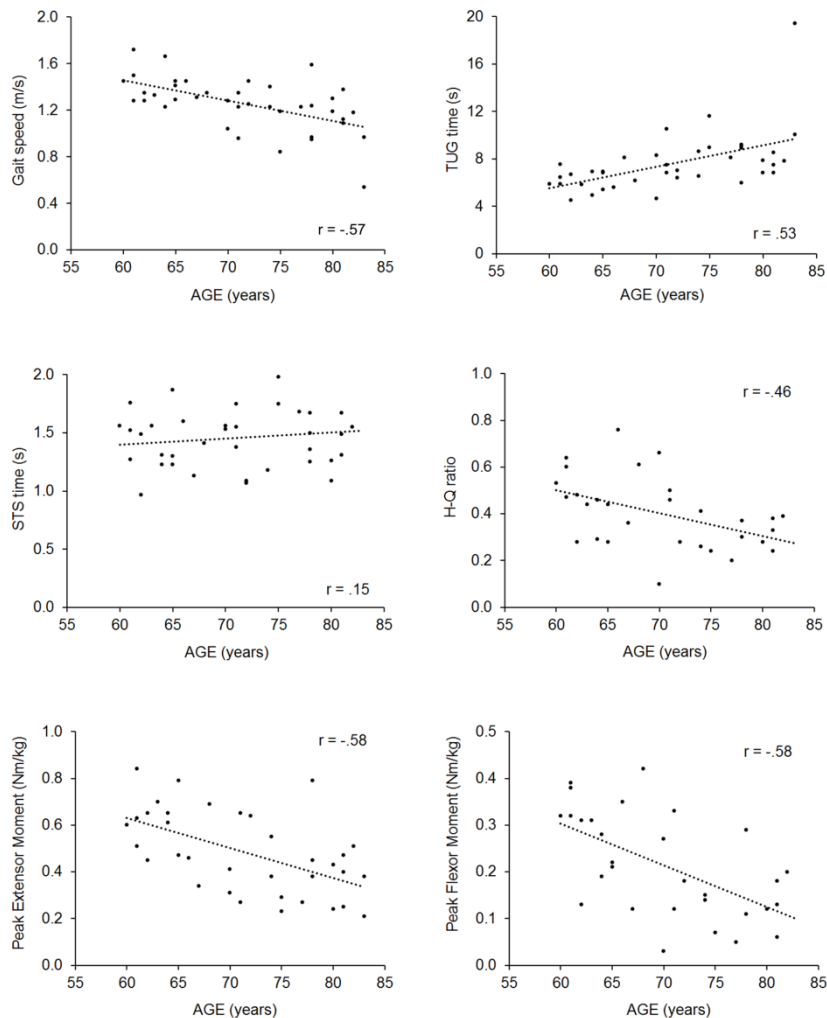
224 [1] Regression model: Age, TUG time - R<sup>2</sup> = 29%, Beta coefficient = 0.121, p = .121

225 [2] Regression model: Age, Mental health: - R<sup>2</sup> = 4%, Beta coefficient = 0.270, p = .267

226 [3] Regression model: Age, MCS: R<sup>2</sup> = 1%, B = -0.086, p = .524

227 Aim 2 – Changes in objective and self-reported physical function

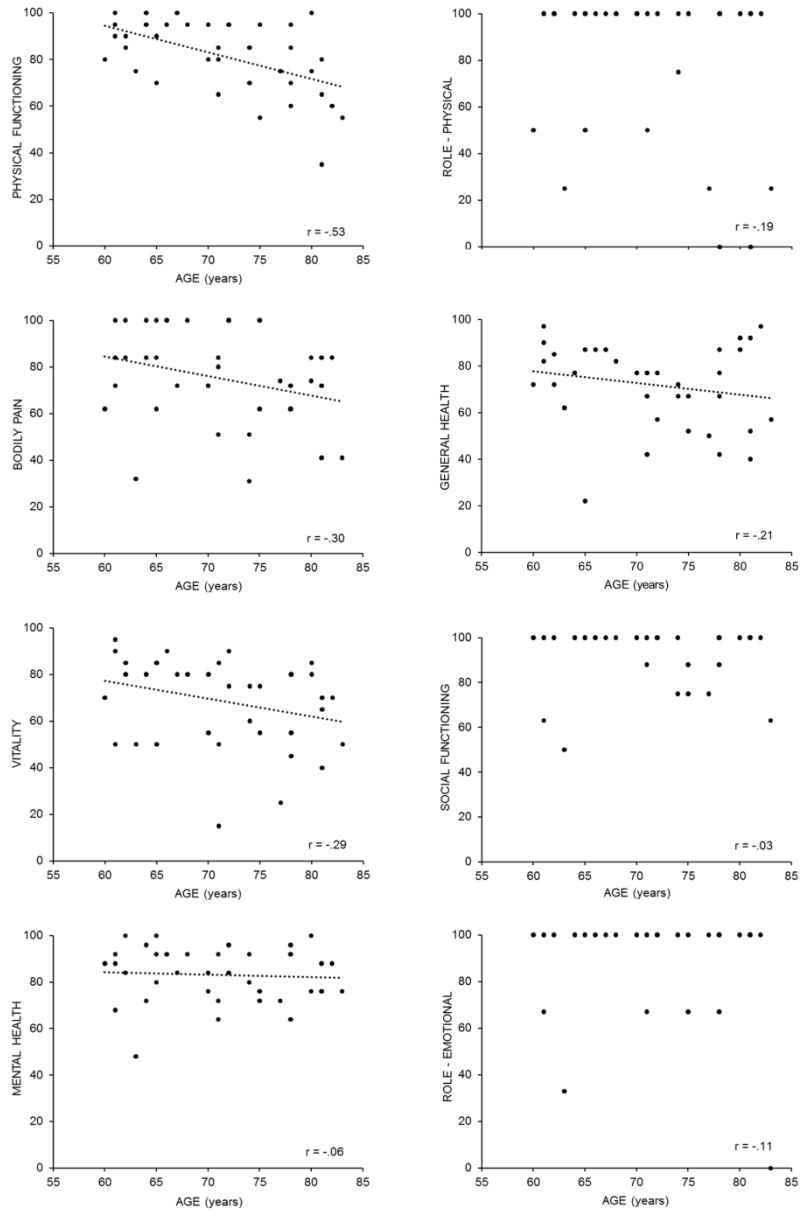
228 Cross-correlations between the outcomes revealed that TUG time strongly correlated with knee  
229 strength ( $r=-.55$  -  $-.68, p \leq .01$ ; Table 2) and was highly correlated with speed ( $r= -.83, p \leq .01$ ). TUG  
230 time was negatively correlated with many of the physical SF-36 sub-scales and the PCS ( $r \geq -$   
231  $.40, p \leq .05$ ). STS correlated well with TUG time ( $r=.38, p \leq .05$ ) and gait speed ( $r=-.35, p \leq .05$ ) but was  
232 not correlated with knee strength. Like TUG time and gait speed, STS time was moderately  
233 correlated with many of the SF-36 subscales ( $r=-.41$  -  $-.54, p \leq .01$ ). Gait speed was positively  
234 correlated with many of the SF-36 variables ( $r=.41-.63, p \leq .05$ ) including all of the physical  
235 components.



236

237 **FIGURE 1** Relationships ( $r$ ) between age and the functional outcome measures studied

238 For completeness graphs are presented with outliers, \*\*  $p \leq .01$  (1-tailed), and \*\*\*  $p \leq .001$  (1-tailed)



239

240 **FIGURE 2** Relationships ( $r$ ) between age and the eight (physical and mental) sub-scales of the SF-

241 36

242 For completeness graphs are presented with outliers, \*  $p \leq .05$

243

244 **TABLE 2** Correlation matrix (r) between all outcome measures studied

		TUG time (s)	STS time (s)	Gait speed (m/s)	HQ ratio (%)	Peak Knee Extensor Moment (Nm/kg)	Peak Knee Flexor Moment (Nm/kg)	SF-36									
								PF	R-P	BP	GH	VT	SF	R-E	MH	MCS	PCS
FUNCTIONAL MEASURES	TUG time (s)		.38	-.83	-.55	-.57	-.68	-.58	-.27	-.40	-.43	-.49	-.30	-.40	-.29	-.31	-.47
	STS time (s)	-		-.35	-.07	-.18	-.12	-.46	-.34	-.43	-.28	-.46	-.54	-.45	-.50	-.50	-.41
	Gait speed (m/s)	-	-		.46	.67	.67	.63	.33	.44	.41	.49	.25	.41	.27	.27	.52
	HQ ratio (%)	-	-	-		.30	.82	.44	.26	.32	.46	.35	.03	-.08	.12	-.04	.45
	Peak Knee Extensor Moment (Nm/kg)	-	-	-	-		.76	.35	.07	.15	.09	.23	.07	.02	.03	.00	.21
	Peak Knee Flexor Moment (Nm/kg)	-	-	-	-	-		.53	.18	.35	.48	.31	.15	-.12	.01	-.14	.47
SELF-REPORTED MEASURES	SF36: Physical Functioning	-	-	-	-	-	-		.71	.74	.55	.55	.34	.60	.10	.12	.90
	SF36: Role – Physical	-	-	-	-	-	-	-		.69	.65	.68	.45	.63	.20	.29	.90
	SF36: Bodily Pain	-	-	-	-	-	-	-	-		.46	.55	.57	.64	.30	.34	.84
	SF36: General Health	-	-	-	-	-	-	-	-	-		.69	.28	.29	.33	.27	.71
	SF36: Vitality	-	-	-	-	-	-	-	-	-	-		.51	.40	.57	.59	.65
	SF36: Social Functioning	-	-	-	-	-	-	-	-	-	-	-		.74	.57	.84	.42
	SF36: Role – Emotional	-	-	-	-	-	-	-	-	-	-	-	-		.22	.59	.64
	SF36: Mental Health	-	-	-	-	-	-	-	-	-	-	-	-	-		.84	.11
	SF36: Mental Component Summary	-	-	-	-	-	-	-	-	-	-	-	-	-	-		.17
	SF36: Physical Component Summary	-	-	-	-	-	-	-	-	-	-	-	-	-	-	-	

245

246 HQ: Hamstrings-to-Quadriceps Ratio, PF: Physical Functioning, R-P: Role-Physical, BP: Bodily Pain, GH: General Health, VT: Vitality, SF: Social Functioning, R-E: Role-Emotional, MH: Mental Health,

247 Light grey shading indicates moderate correlations  $r = 0.4-0.6$   $p < .05$ , and dark grey shading indicates strong correlations  $r = 0.7-1.0$   $p < .05$ .

248

## 249 **DISCUSSION**

250 This study used linear regression to quantify the changes in objective and self-reported function  
251 that were attributable to age alone. This is a novel approach that furthers our understanding  
252 beyond that of previous studies which have assessed functional loss using a single clinical  
253 assessment (2, 3, 21, 24, 25, 39) or a battery of assessments according to broad pre-defined age  
254 groupings (1, 3, 40-42). This study found that the pattern of age-related functional losses can be  
255 estimated using linear regression, thereby enhancing our understanding of the rate of decline  
256 throughout older age. Furthermore, large within-group variability (represented by the standard  
257 deviation) was observed for many of the outcomes presented, indicating that categorising  
258 individuals across large age ranges, as has been common in previous research(43, 44), leads to  
259 considerable variation and limited information about age-related functional decline.

260

### 261 *Aim 1 - Estimation of annual changes in health and physical function*

262 Overlapping 95%CI for estimated annual changes in all of the objective outcomes (except for STS)  
263 and the Physical Functioning and Physical Component Summary of the SF-36 (Table 1) indicate  
264 that gradual losses due to biological ageing processes appear to occur at similar rates for which  
265 age has been shown to explain significant variation ( $R^2=14-34\%$ ). This is in agreement with  
266 previous research demonstrating that age was a major contributor, explaining significant variation  
267 in TUG time ( $R^2=60\%$ ), gait speed ( $R^2=63\%$ ) and timed STS ( $R^2=37\%$ )(1). While the convenience  
268 sample in that study(1) showed gradual decline over a large age range (66-101years), both men  
269 and women were tested which may have affected the point estimates due to gender differences in  
270 musculoskeletal function/capacity(5, 6) and relative life expectancy(8). Our study has  
271 demonstrated that significant annual losses in function occur within a cohort of healthy older  
272 women and further analyses should be repeated with men for comparison. To our knowledge,  
273 Lusardi et al.'s study(1) is the only study that has taken a similar approach to understanding age-  
274 related decline in a battery of motor function indices. Other studies have quantified losses in a

275 similar fashion, for musculoskeletal strength (45) but have not investigated relative annual decline  
276 for a range of functional characteristics.

277

278 It is noteworthy that greater age-induced losses were observed for the knee flexors compared with  
279 the extensors, and this is in agreement with longitudinal observations of older women(45). Those  
280 findings, along with our present data, indicate that the smaller flexor muscles experience greater  
281 strength losses compared to the larger anti-gravity extensor group. Accordingly, the point  
282 estimates presented in this study indicate that the hamstrings-to-quadriceps (H:Q) ratio reduced  
283 with age, with an annual loss of 2.0%. This suggests that the strength difference between this  
284 antagonistic pair became larger with age. Such declines may impact adversely on the ability to  
285 negotiate obstacles and stairs safely; execute postural transitions; bend down to a lower level; and  
286 ultimately knee joint stability. It should be noted that the knee flexion moments of five of the oldest  
287 participants were excluded from all analyses because they were unable to achieve the constant  
288 target velocity (isovelocity phase). This was despite multiple trials and verbal encouragement, and  
289 was most likely because they lacked muscle power to accelerate the dynamometer lever arm  
290 adequately. Consequently, the reported knee flexion moments for participants aged >75 years are  
291 likely overestimated compared to the population and the annual decline for knee flexion moment  
292 and H:Q ratio are likely underestimated. We consider this to further demonstrate the significant  
293 age-related weakness in the oldest old (particularly for knee flexor tasks). However, even at the  
294 magnitudes observed considerable losses were identified that in accumulation could restrict  
295 mobility and independent functioning. The expansion of this work to other antagonistic muscle  
296 pairs (hip and ankle) may help to define joint functionality and inform the nature of age-related  
297 reciprocal muscle strength loss. While the accumulated annual changes in knee strength with age  
298 are of clinical significance, it must be highlighted that in some cases, cross-sectional studies have  
299 reportedly underestimated strength losses compared to longitudinal research(45).

300

301 Interestingly, age explained moderate levels of variance in Physical Functioning and the PCS,  
302 which was of a similar magnitude to the measured physical decline observed in gait speed, TUG

303 time and knee strength. Age did not explain significant variance in any other SF-36 sub-scale  
304 suggesting that some aspects of the SF-36 may reveal changes related to other factors such as  
305 personality type, or demonstrate inconsistencies due to individual perception. A self-reporting  
306 survey results in perceived ability and/or status rather than actual task performance, assessed  
307 objectively. Although self-reporting general health scales have been suggested to predict functional  
308 decline accurately(46), the under- or over-reporting of physical status has been linked to  
309 personality traits and levels of self-awareness(47). This study has shown that, in a sample of  
310 healthy older women with no prior falls history, self-reported function estimated measured  
311 performance very accurately. We found the same annual loss for gait speed and for the Physical  
312 Functioning sub-scale of the SF-36 (1.2%/year). 95%CI overlapped for these variables and were  
313 small, indicating that within this cohort the changes were predicted very precisely. This was likely  
314 indicative of the participants' good health and independent living status.

315

316 In summary, accumulative losses in function have been demonstrated in the current study. The  
317 year-on-year changes in function presented may appear to be small and thus not clinically  
318 significant. However, when considering the accumulation of these changes across several years  
319 and in relation to critical thresholds proposed within the literature (For example, gait speeds of  
320 <1.0m/s(48) and TUG times of >14s(13)) the optimal time to intervene may be planned to  
321 attenuate losses before overall function is affected clinically. Larger population-based studies are  
322 required to substantiate the declines presented in this study and then national databases may be  
323 developed and used to monitor functional/ global health changes to estimate demographic health  
324 and future costs.

325

326 *Aim 2 – Changes in objective and self-reported physical function*

327 Using gait speed as a clinical outcome is advantageous due to its high test-retest reliability(2, 5),  
328 as well as the significant correlations other outcomes(1) and deterioration with age(2). This study



329 found that that in addition to speed, TUG time reflects the functional declines in many ADL. In fact,  
330 utilising the TUG test in clinical practice may be advantageous due to the limited space/ equipment  
331 and expertise required compared with the space required to attain, and record speed from, steady-  
332 state gait. However, both of these objective outcomes should be included routinely as part of a  
333 normal health check-up and physical assessment of older women. Reduced performance on these  
334 outcomes may be caused by declining knee extensor strength which contributes heavily to both  
335 measures (lower limb stability and forward continuance during level gait; and raising the body from  
336 a seated position). Measured leg strength is not currently included on the list of validated measures  
337 provided by the CSP. This is likely due to the dynamometry equipment and technical expertise  
338 required for data acquisition. A viable compromise may include quantifying muscle strength  
339 manually given its widespread use within a clinical setting(49, 50). Reliable, valid data may be  
340 obtained from such measures(51, 52) providing that recommendations such as those proposed by  
341 the International College of Applied Kinesiology are adhered to(53). However, extra care must be  
342 taken when constructing controlled testing conditions for use with large age ranges given that  
343 some of the oldest individuals appear unable to perform at higher joint angular velocities.  
344 Furthermore, slower gait speeds may result from age-associated muscle weakness(54), and more  
345 specifically knee extensor strength loss (as indicated by the findings in this study). Therefore,  
346 reduced functioning when standing from sitting (TUG) combined with deteriorating gait speeds,  
347 both relatively simple measures to obtain, may provide an early indication of knee extensor  
348 weakness which consequently will adversely affect overall physical function. To this end, measures  
349 of gait speed and TUG time proved to be informative markers indicative of functional decline,  
350 related most strongly to performance across a range of ADLs, and thus should continue to be  
351 collected as part of routine assessment in outpatients, clinics and physiotherapy/ rehabilitation.

352

353 Measuring STS performance did not reveal functional losses above and beyond that of comfortable  
354 gait speed, TUG time and knee strength. Thus, performing the STS is unlikely to further enhance  
355 our understanding of annual musculoskeletal changes in performance when used in combination  
356 with other outcomes. Rarely, do we perform a single postural transition in isolation and STS time

357 may be criticised for its lack of ecological validity. Moderate correlations were observed between  
358 STS time and some of the psychological subscales of the SF-36 and the role of psychological  
359 status and STS time has been confirmed previously(55).

360

361 The results of this study emphasise that there was a continuous decline in function throughout  
362 older age. These musculoskeletal losses occurred even in a sample of healthy older women, for  
363 whom functional decline appeared to be linear. Gait speed and TUG time were reaffirmed as  
364 markers indicative of functional decline and related most strongly to performance across a range of  
365 ADLs. Considering their cost- and time-effectiveness and strong correlation with many other  
366 outcomes, gait speed and TUG should be incorporated into routine clinical and geriatric  
367 assessments starting from middle-age as declines occur in even healthy older women beyond 60  
368 years of age. The significant correlations between H:Q ratio and TUG time ( $r=-.55$ ) and gait speed  
369 ( $r=.46$ ) further substantiate their suitability for clinicians to obtain during routine assessments with  
370 older adults. However, because knee flexor strength does not contribute to TUG time and gait  
371 speed as much as extensor strength, additional assessments may be required to identify flexor  
372 strength and H:Q ratio losses. The predicted yearly decline in knee flexor strength, which was  
373 greater than for the knee extensors, has important implications for the safe execution of many  
374 functional tasks which may not be otherwise highlighted by losses in gait speed and TUG time  
375 alone. Consequently, this should be addressed in exercise interventions for older adults, as the  
376 knee flexors may be 'neglected' in primarily anti-gravity based exercises.

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