1 THIS IS A NON-FINAL VERSION OF AN ARTICLE PUBLISHED IN FINAL

- 2 FORM IN Medicine and Science in Sports and Exercise
- 3 Moving forward with backwards compatibility: Translating wrist accelerometer data
- 4 Short title: Translating wrist accelerometer data
- 5 Rowlands AV, ^{1,2,3} Cliff DP, ⁴ Fairclough SJ, ^{5,6} Boddy LM, ⁷ Olds TS, ³ Parfitt G, ³
- 6 Noonan RJ, Downs SJ, Knowles ZR, Beets MW⁸
- 7 1. Diabetes Research Centre, University of Leicester, Leicester General Hospital,
- 8 Leicester, UK
- 9 2. NIHR Leicester-Loughborough Diet, Lifestyle and Physical Activity
- 10 Biomedical Research Unit, UK
- 3. Alliance for Research in Exercise, Nutrition and Activity (ARENA), Sansom
- 12 Institute for Health Research, Division of Health Sciences, University of South
- 13 Australia, Adelaide, Australia
- 4. Early Start Research Institute, School of Education, Faculty of Social
- Sciences, University of Wollongong, Wollongong, NSW, Australia
- 5. Department of Sport and Physical Activity, Edge Hill University, Ormskirk, UK
- 6. Department of Physical Education and Sport Sciences, University of Limerick,
- 18 Limerick, Ireland
- 7. Physical Activity Exchange, Research Institute for Sport and Exercise
- Sciences, Liverpool John Moores University, Liverpool, UK
- 8. Arnold School of Public Health, Department of Exercise Science, University
- of South Carolina, USA
- 23 Corresponding author: Alex Rowlands, Diabetes Research Centre, University of
- Leicester, Leicester General Hospital, Leicester, LE5 4PW, UK.
- alex.rowlands@leicester.ac.uk.

27	Purpose: To provide a means for calibrating raw acceleration data from wrist-worn
28	accelerometers in relation to past estimates of children's moderate-to-vigorous
29	physical activity (MVPA) from a range of cut-points applied to hip-worn ActiGraph
30	data. Methods: This is a secondary analysis of three studies with concurrent 7-day
31	accelerometer wear at the wrist (GENEActiv) and hip (ActiGraph) in 238 children
32	aged 9-12 years. The time spent above acceleration (ENMO) thresholds of 100, 150,
33	200, 250, 300, 350 and 400 mg from wrist acceleration data (≤5 s epoch) was
34	calculated for comparison to MVPA estimated from widely used children's hip-worm
35	ActiGraph MVPA cut-points (Freedson/Trost 1100 counts per minute (cpm); Pate
36	1680 cpm; Evenson 2296 cpm; Puyau 3200 cpm) with epochs of ≤5, 15 and 60 s.
37	Results: The optimal ENMO thresholds for alignment with MVPA estimates from
38	ActiGraph cut-points determined from 70% of the sample and cross-validated with
39	the remaining 30% were: Freedson/Trost = ENMO 150+ mg, irrespective of
40	ActiGraph epoch (ICC≥0.65); Pate = ENMO 200+ mg, irrespective of ActiGraph
41	epoch (ICC \geq 0.67); Evenson = ENMO 250+ mg for \leq 5 s and 15 s epochs (ICC \geq 0.69)
42	and ENMO 300+ mg for 60 s epochs (ICC=0.73); Puyau = ENMO 300+ mg for \leq 5 s
43	epochs (ICC=0.73), ENMO 350+ mg for 15 s epochs (ICC=0.73), ENMO 400+ mg
44	for 60 s epochs (ICC=0.65). Agreement was robust with cross-validation ICCs=0.62-
45	0.71 and means within 7.8 ±4.9% of MVPA estimates from ActiGraph cut-points,
46	except Puyau 60 s epochs (ICC=0.42). Conclusion: Incremental ENMO thresholds
47	enable children's acceleration data measured at the wrist to be simply and directly
48	compared, at a group level, to past estimates of MVPA from hip-worn ActiGraphs
49	across a range of cut-points.
50	Keywords: Physical activity, children, MVPA, ActiGraph, GENEActiv, cut-point

Introduction

51

52

53

54

55

56

57

58

59

60

61

62

63

64

65

66

67

68

69

70

71

72

73

74

75

Objective measures of physical activity, specifically uniaxial hip-worn accelerometers, were introduced into national surveys in the US (National Health and Nutrition Examination Survey, NHANES) in 2003 (29), Canada (Canada Health Measures Survey) in 2007 (7,8) and the UK (Health Survey for England) in 2008 (17). Also in 2008, the International Children's Accelerometry Database (ICAD) was initiated: a compilation of accelerometer-derived estimates of children's physical activity from a wide range of studies, settings, and countries (28). The accelerometers employed in these surveys and studies converted accelerations into proprietary counts stored in 5-60 s epochs and time accumulated in moderate-to-vigorous physical activity (MVPA) was subsequently estimated. Over the past decade there have been rapid developments in accelerometry resulting in the commercial availability of triaxial microelectromechanical (MEMS) accelerometers that continuously sample and store raw accelerations at up to 100 Hz, such as the ActiGraph GT3X+ and the GENEActiv. There has also been a move to 24 h wear protocols with wrist-wear to maximize compliance (2,9,14) and facilitate measurement of the full spectrum of physical behaviours (physical activity, sedentary behavior and sleep) (6). As a result, since 2011, wrist-worn ActiGraph GT3X+ monitors that collect and store raw accelerations at 100 Hz have been used in NHANES (30). Other large-scale adult (2,9,21) and children's (9,10,20,34) studies are also employing 24 h wrist-worn accelerometer protocols using the GENEActiv. As the ActiGraph GT3X+ and the GENEActiv store raw accelerations rather than proprietary counts, their data should, theoretically, be comparable. Output from the

GENEActiv and the Actigraph GT3X+, when processed and calibrated identically using the open source package GGIR (32,33) in R [http:/cran.r-project.org], have high agreement for acceleration magnitudes >50-80 mg, indicative of light activity and MVPA, although not for lower acceleration magnitudes indicative of sedentary time (27).

Advances in measurement methods (e.g. self-report to objective measurement) and/or measurement technologies (e.g. proprietary count uniaxial accelerometers to raw acceleration triaxial accelerometers) bring reduced bias, improved precision and enhanced measurement opportunities (30), but at a cost of limited comparability to past data. There is a wealth of MVPA data on children estimated from uniaxial hip-worn ActiGraphs (28,29) and it is desirable to use these data to: contextualize future estimates of MVPA; map trends in physical activity; compare effectiveness of past and present interventions; and understand the clinical significance of intervention changes in PA, by contextualizing current data with the extant historical evidence on the impact of physical activity on health. To complicate comparisons further, hip-worn ActiGraph data have been analyzed using an extensive range of cut-points leading to widely varying estimates of MVPA even for the same dataset (4,5,15).

The purpose of this study is to provide a means for quickly and simply comparing raw acceleration data from wrist-worn accelerometers at a group level to past estimates of children's MVPA from a range of cut-points applied to hip-worn ActiGraph data. To do this, we used data from three studies that have concurrent 7-day accelerometer wear at the wrist (GENEActiv) and hip (ActiGraph) to determine and cross-validate the acceleration magnitudes most closely associated with established MVPA cut-

points. As the GENEActiv and ActiGraph GT3X+ have high agreement for accelerations indicative of light activity and MVPA (27), the results will be applicable to studies measuring raw triaxial accelerations at the wrist in children with either the ActiGraph GT3X+ or the GENEActiv.

Methods

This is a secondary data analysis using data from three studies: 1) 58 children, aged 10-12 years, recruited from primary schools in South Australia (26); 2) 129 children, aged 9-10 years, recruited from primary schools in Liverpool, UK (12); 3) 81 children, aged 9-11 years, recruited from one primary school in Liverpool, UK. The appropriate university research ethics committee approved each study. Written informed consent and assent were obtained from the parents/guardians and children, respectively. Height was measured to the nearest 0.1 cm and body mass to the nearest 0.1 kg.

Assessment of activity

Free-living physical activity was measured by concurrent wear of the GENEActiv on the non-dominant wrist and the ActiGraph GT3X+ positioned above the right hip, on an elasticated belt worn around the waist, for seven consecutive days. In study 1, children were requested to wear both monitors day and night, removing the hip-worn ActiGraph for water-based activities only. In studies 2 and 3, children were requested to wear both monitors at all times except when sleeping or during water-based activities.

1	2	6

Accelerometers

The GENEActiv is a triaxial accelerometry-based activity monitor with a dynamic range of +/- 8g (Gravity Estimator of Normal Everyday Activity, ActivInsights Ltd, Cambridgeshire, UK). The ActiGraph GT3X+ is a triaxial accelerometry-based activity monitor with a dynamic range of +/- 6 g (ActiGraph LLC, Pensacola, FL, USA). Study 1: The GENEActivs were initialized to collect data at 87.5 Hz and data uploaded using GENEActiv PC software version 2.2. The ActiGraphs were initialized to collect data at 80 Hz and data uploaded using Actilife version 6.5.3. Data were collected between April and December 2012. Studies 2 and 3: The GENEActivs and ActiGraphs were both initialized to collect data at 100 Hz and data uploaded using GENEActiv PC software version 2.2 and Actilife version 6.11.4, respectively. Study 2 data were collected between January and May 2014 and study 3 data were collected in January and February 2015.

Data processing

Wrist-worn GENEActiv (raw acceleration) GENEActiv .bin files were analysed with R-package GGIR version 1.2-0 (http://cran.r-project.org) (32,33). Signal processing in GGIR includes the following steps: 1. Autocalibration using local gravity as a reference (32); 2. Detection of sustained abnormally high values; 3. Detection of non-wear; 4. Calculation of the average magnitude of dynamic acceleration, i.e. the vector magnitude of acceleration corrected for gravity (Euclidean Norm minus 1 g, ENMO) over user-defined s epochs:

ENMO = $\sum \sqrt{x^2 + y^2 + z^2} - g$ with negative values set to zero. In study 1,

ENMO was averaged over 5 s epochs; in studies 2 and 3, ENMO was averaged over 1

s epochs. As studies applying GGIR to wrist accelerometer data have used both 1 s

(12) and 5 s epochs (9), inclusion of both epochs increases the generalizability of the

findings.

156

157

159

160

161

162

163

164

165

166

167

154

Files were excluded from all analyses if post-calibration error was greater than 0.02~g

158 (9) and individual days were classified as invalid and excluded if wear-time was

insufficient (16 h for the 24 h protocol in study 1, 10 h for the waking wear protocol

in studies 2 and 3). Detection of non-wear has been described in detail previously

(See 'Procedure for non-wear detection' in supplementary document to van Hees et

al. (33)). In brief, non-wear is estimated based on the standard deviation and value

range of each axis, calculated for 60 min windows with 15-min moving increments. If

for at least 2 out of the 3 axes the SD is less than 13 mg or the value range is less than

50 mg the time window is classified as non-wear. The default non-wear setting was

used, i.e. invalid data were imputed by the average at similar timepoints on different

days of the week

168

169

170

171

172

The distribution of time spent across ENMO levels in 50 mg resolution (0-50 mg, 50-

100 mg..... ≥400 mg) was calculated using the argument 'ilevels' from the GGIR

package. The time spent above thresholds of 100, 150, 200, 250, 300, 350 and 400 mg

was calculated for comparison to widely used hip-worn ActiGraph MVPA cut-points.

173

Hip-worn ActiGraph (counts)

175

Data were analyzed using Actilife version 6.13.0. The raw.gt3x files were summarized into uniaxial (vertical) proprietary counts in 1 s, 5 s, 15 s and 60 s epochs, resulting in four ActiGraph files for analysis per participant. Non-wear was defined as 60 min of consecutive zero counts, with an allowance for 1-2 min of counts between 0 and 100 (29). Individual days were classified as invalid and excluded if wear-time was insufficient (16 h for the 24 h protocol in study 1, 10 h for the waking wear protocol in studies 2 and 3).

Each file was analyzed with four widely-used MVPA cut-points: very low (1100 cpm (counts per minute), approximately equivalent to the cut-point for an 11 y old (3 METs) using the age-specific criteria of the Freedson group, published by Trost et al. (31)); low (1680 cpm, Pate et al. (23)); medium (2296 cpm, Evenson et al. (11)); high (3200 cpm, Puyau et al. (24)). This resulted in 16 outputs per participant: MVPA classified using very low, low, medium and high cut-points, with each cut-point applied to data integrated into 1 s, 5 s, 15 s and 60 s epochs.

Data analysis

For each participant, days were only included if classified as valid for both the wrist-worn GENEActiv and hip-worn ActiGraph; therefore to be included a participant needed a minimum of one day where both the ActiGraph and GENEActiv recorded sufficient wear time. The daily means for all output variables were taken for each participant. For data from study 1, GENEActiv 5 s epoch outputs were compared to the ActiGraph 5 s, 15 s and 60 s epoch outputs. For data from studies 2 and 3, the GENEActiv 1 s epoch files were compared to the ActiGraph 1 s, 15 s and 60 s

epochs. The 5 s data from study 1 and the 1 s data from studies 2 and 3 were designated a \leq 5 s epoch.

Descriptive statistics (mean \pm SD) were calculated for all variables. Data from studies 1 and 2 (approximately 70% of the total sample) were analyzed with data from study 3 reserved for cross validation. The wrist-worn GENEActiv ENMO thresholds (100+, 150+, 200+, 250+, 300+, 350+, 400+ mg) which most closely approximated time accumulated in each of the hip-worn ActiGraph MVPA cut-points (very low, low, medium, high) for each epoch length (\leq 5 s, 15 s, 60 s) were examined with a series of limits of agreement (LoA) analyses (3) and intra-class correlations (ICC, single measures, absolute agreement) with 95% confidence intervals (CI).

For each hip-worn ActiGraph MVPA cut-point / epoch combination, the wrist-worn ENMO threshold with the closest agreement was selected and the agreement between these optimal pairings tested in the independent cross-validation sample. The distributions for each of the optimal pairings were illustrated on kernel density plots (bandwidth = 10) for the total sample (data from studies 1, 2 and 3 combined).

Results

Demographic data, by study, are presented in Table 1. The final sample size was 238 (Test sample N=159, Cross-validation sample N=79) with 30 participants excluded due to no days of concurrent valid wear for both monitors. Figure 1 shows the time recorded in each of the intensity categories by the hip-worn ActiGraph (very low, low, medium and high MVPA cut-points) and the wrist-worn GENEActiv (100+,

```
226
       150+, 200+, 250+, 300+, 350+, 400+ mg ENMO thresholds) by epoch (ActiGraph < 5
227
       s, 15 s, 60 s; GENEActiv <5s) for the total sample.
228
229
       Test sample
230
231
       The agreement between each wrist-worn GENEActiv ENMO threshold and each hip-
232
       worn ActiGraph MVPA cut-point is shown for each epoch length in Table 2. The
233
       ENMO threshold with the highest agreement for each ActiGraph MVPA cut-point /
234
       epoch combination is highlighted in bold in Table 2. The optimal wrist-worn ENMO
235
       thresholds for comparison to hip-worn ActiGraph MVPA cut-points were:
236
           • very low MVPA ActiGraph cut-points (1100 cpm, Trost et al. (31))
237
                  \circ ENMO 150+ mg, irrespective of the ActiGraph epoch (ICC > 0.65,
238
                     mean bias (ENMO - ActiGraph) = -2.9 \text{ to } -18.0 \text{ min, } (-2.7 \text{ to } -14.9\%)
239
                     of mean MVPA));
240
          • low MVPA ActiGraph cut-points (1680 cpm, Pate et al. (23))
241
                  o ENMO 200+ mg, irrespective of the ActiGraph epoch (ICC \geq 0.67,
242
                     mean bias = -4.1 to -10.7 min (-5.4 to -13.0% of mean MVPA));
243
              medium MVPA cut-points (2296 cpm, Evenson et al. (11))
244
                  \circ ENMO 250+ mg for <5 s and 15 s epochs (ICC > 0.69, mean bias = -
245
                     3.0 to -7.3 min (-5.4 to -12.0% of mean MVPA))
246
                  \circ ENMO 300+ mg for 60 s epochs (ICC = 0.73, mean bias = -5.0 min (-
247
                     10.6% of mean MVPA));
248
            high MVPA cut-points (3200 cpm, Puyau et al. (24))
249
                  \circ ENMO 300+ mg for <5 s epochs (ICC = 0.73, mean bias = +1.8 min
250
                     (+4.7% of mean MVPA))
```

251	\circ ENMO 350+ mg for 15 s epochs (ICC = 0.73, mean bias = +2.7 min
252	(+8.7% of mean MVPA))
253	\circ ENMO 400+ mg for 60 s epochs (ICC = 0.65, mean bias = +6.5 min
254	(+28.6% of mean MVPA)).
255	
256	Cross-validation
257	
258	The agreement of each of these optimal pairings of wrist-worn ENMO threshold and
259	hip-worn ActiGraph MVPA cut-point was tested in the cross-validation sample
260	(Table 3, Figure 2). Agreement was robust with ICC's similar to the test sample for
261	15 s epochs (very low, low and medium MVPA cut-points, mean bias = $ 4.9 \pm 0.9\%$
262	of mean MVPA) and \approx 0.01-0.11 lower than the test sample (0.61 to 0.71, mean bias =
263	$ 8.9 \pm 4.8\%$ of mean MVPA) for other MVPA cut-point / epoch combinations, except
264	for the high MVPA cut-point $\!\!\!/\!\!\!/ 60$ s epoch where the ICC was considerably reduced
265	(0.42). The mean biases and 95% limits of agreement were also similar in magnitude
266	to the test sample. However, the values of the mean bias for specific pairings were not
267	consistent between the test sample and the cross-validation sample.
268	
269	The distribution of the ActiGraph and ENMO data for each of the optimal pairings is
270	shown on kernel density plots for the total sample, Figure 3. The columns represent
271	cut-points (left to right: very low, low, medium, high) and the rows represent
272	ActiGraph epochs (top to bottom: ≤ 5 s, 15 s, 60 s). The agreement statistics for the
273	total sample are shown in Supplemental Digital Content 1.
274	
275	

Discussion

Rapid progress in accelerometer technology has led to changes in the data collected and study protocols followed, with a shift from uniaxial proprietary count outcomes collected using accelerometers worn at the hip to triaxial raw accelerations measured using wrist-worn accelerometers (30). We have developed a quick and simple method to facilitate the comparison of group level estimates of children's MVPA from uniaxial hip-worn count-based ActiGraphs to triaxial raw acceleration data measured at the wrist processed using the open source R-package, GGIR (32,33). The method was developed using the GENEActiv wrist-worn accelerometer, but evidence suggests it will also be applicable to raw acceleration measured at the wrist using the ActiGraph and processed in GGIR (27).

Mean biases for optimal pairings of ENMO thresholds and ActiGraph MVPA cutpoints were relatively low (test sample: mean bias = $|9.4| \pm 4.2\%$ of mean MVPA; cross-validation sample: mean bias = $|7.8| \pm 4.9\%$ of mean MVPA) indicating good group level agreement, excluding high ActiGraph MVPA cut-points assessed using a 60 s epoch where mean bias was high relative to the low means (29% in the test sample, 60% in the cross-validation sample). Similarly, the ICC's for optimal pairings were all between 0.61 and 0.76 in the test and cross-validation sample, indicating good agreement (13), with the exception of the high ActiGraph MVPA cut-points assessed using a 60 s epoch in the cross-validation sample (ICC = 0.42). The 95% limits of agreement were moderate to large indicating that individual level

comparisons are not advised. The MVPA recorded in the cross-validation sample was lower than the test samples, in particular when applying high cut-points with a 60 s epoch (Figures 1 and 2); this may have contributed to the lower robustness for the high cut-point/60 s epoch combination. Hildebrand et al. (16) developed an MVPA threshold of approximately 200 mg for use with wrist-worn ActiGraph and GENEActiv accelerometers. Based on the current findings, MVPA determined by applying the 200 mg threshold to wrist-worn accelerometer data should compare best to MVPA determined from low cut-points (23) applied to hip-worn ActiGraph data, irrespective of epoch. Overall, the cross-validation suggests that agreement may be closest when comparing ENMO 150+, 200+ and 250+ thresholds to MVPA estimated from ActiGraph 15 s epoch data processed using very low, low and medium cut-points, respectively.

The potential for application of these comparisons is extensive. By 2010, over 46000 physical activity datasets from hip-worn ActiGraphs had been collated in the ICAD, approximately 19000 from children aged 9-12 y, (28). More recently, the International Study of Childhood Obesity, Lifestyle and the Environment (ISCOLE) collected data on 6000 children, aged 9-11 y from 12 countries across five diverse regions of the world using hip-worn ActiGraphs (18). The latter study collected triaxial raw acceleration data using ActiGraph GT3X+ and has developed novel analytical tools for application to the raw acceleration data, e.g. to determine sleep duration (1), but as the hip was the measurement site these data have also been summarized in proprietary counts and analyzed using count cut-points (19). Since NHANES moved to assessing physical activity using triaxial raw acceleration data measured at the wrist for the NHANES cycles 2011-2012 and 2013-2014 (30), many

other large studies have also used wrist-worn accelerometers. For example, data have already been collected in: ≈4000 children, aged 9-11 v, in the Child Health Checkpoint (Melbourne, Australia (34)); ≈1800 girls, aged 11-14 y, in Girls Active (Leicester, UK (10)); ≈1000 children, aged 8-11 y in the Cork Children's Lifestyle Study (Ireland (20)); and ≈4000 children aged 7 y in the Pelotas Birth cohort (Brazil (9)). The comparisons presented will facilitate interpretation of these data in relation to past estimates of children's MVPA, e.g. from NHANES, ICAD and ISCOLE. The data collated for this study came from three different sources and were collected using two differing protocols. Study 1 took place in South Australia, used a 24 h wear protocol and summarized the GENEActiv ENMO data in 5 s epochs. Studies 2 and 3 took place in the UK, used a waking time only protocol and summarized the ENMO data in 1 s epochs. While the results were similar across studies and the crossvalidation (study 3 data) showed the agreement statistics were robust, these differences limit the internal validity of the study. However, the external validity is enhanced, as results are applicable to ENMO data collected in 1 s and 5 s epochs using either a waking or 24 h protocol. Given the outcome of interest was MVPA it is not surprising that the use of a waking or 24 h protocol did not impact on the results.

326

327

328

329

330

331

332

333

334

335

336

337

338

339

340

341

342

343

344

345

346

347

348

349

350

ActiGraph epochs of ≤ 5 s, 15 s and 60 s were considered, whereas ENMO data were only summarized into ≤ 5 s epochs. The use of longer epochs in the past was due to the memory limitations of accelerometers (30). Accelerations were integrated onboard the accelerometer and stored in epochs, normally 60 s epochs, to ensure one week of data could be stored before downloading the data. Due to technological progress onboard memory is no longer a problem and raw acceleration data collected at 100 Hz

can be stored for one week. Therefore it is unlikely that epochs longer than the default 5 s epoch in GGIR will be used, particularly when assessing children's activity where the typical sporadic activity patterns are best captured using short epochs (22). It should be noted that the participants in this study were from a relatively narrow age range and the results cannot be generalized beyond the 9-12 y age group tested.

In summary, this study indicates that, in 9-12 y old children, time accumulated above the appropriate incremental ENMO threshold has good agreement at a group level with a range of widely used very low to high ActiGraph MVPA cut-points. It is important to note this is a simple pooled-data comparison study that enables group level comparisons, but individual level comparisons are not advised. We recommend that when processing triaxial raw acceleration wrist accelerometer data using GGIR, the times accumulated above ENMO thresholds ranging from \geq 100 to \geq 400 mg, or in incremental acceleration bins (e.g. 9), are presented. As well as providing an activity profile, this will enable the reader to quickly and simply compare the findings to past estimates of children's MVPA from hip-worn ActiGraph data across a range of widely used cut-points.

Acknowledgements

Study 1 was funded by the University of South Australia and Studies 2 and 3 were funded by Liverpool John Moores University. AR is with the National Institute for Health Research (NIHR) Diet, Lifestyle & Physical Activity Biomedical Research Unit based at University Hospitals of Leicester and Loughborough University, the National Institute for Health Research Collaboration for Leadership in Applied Health

376	Research and Care – East Midlands (NIHR CLAHRC – EM) and the Leicester
377	Clinical Trials Unit. The views expressed are those of the authors and not necessarily
378	those of the NHS, the NIHR or the Department of Health. DPC is funded by an
379	Australian Research Council (ARC) Discovery Early Career Researcher Award
380	(DE140101588). The results of the present study do not constitute endorsement by the
381	authors or the American College of Sports Medicine of the products described in this
382	article. The results of the study are presented clearly, honestly, and without
383	fabrication, falsification, or inappropriate data manipulation. There are no conflicts of
384	interest.

385 **References**

- Barreira TV, Schuna JM, Jr., Mire EF, et al. Distinguishing children's
 nocturnal sleep using 24-hour waist accelerometry. *Med Sci Sports Exerc* 2015; 47: 937–943.
- 390 2. Bell JA, Hamer M, van Hees VT, Singh-Manoux, A, Kivimäki, Sabia S.
- Healthy obesity and objective physical activity. *Am Soc Nutr* 2015 doi:
- 392 10.3945/ ajcn.115.110924.
- 393 3. Bland JM, Altman GA. Statistical methods for assessing agreement between two methods of clinical measurement. *Lancet*. 1986;1(8476)307-310.
- Bornstein DB, Beets MW, Byun W et al. Equating accelerometer estimates of
 moderate-to-vigorous physical activity: in search of the Rosetta Stone. *J Sci Med Sport* 2011; 14: 404-410.
- 5. Brazendale K, Beets MW, Bornstein DB et al. Equating accelerometer
 estimates among youth: The Rosetta Stone 2. *J Sci Med Sport* 2016; 19: 242 249.
- Buman, M.P., Hu, F., Newman, E., Smeaton, A.F., Epstein, D.R. Behavioral
 periodicity detection from 24 h wrist accelerometry and associations with
 cardiometabolic risk and health-related quality of life. *BioMed Research Int* 2016; 2016;4856506. doi: 10.1155/2016/4856506. Epub 2016 Jan 31.
- Colley RC, Garriguet D, Janssen I, Craig, C.L., Clarke, J., Tremblay, M.S.
 Physical activity of Canadian adults: Accelerometer results from the 2007 to
 2009 Canadian Health Measures Survey. *Health Reports* (Statistics Canada,
 Catalogue 82-003) 2011; 22(1): 7-14.

- 8. Colley, R.C., Garriguet, D., Janssen, I., Craig, C.L., Clarke, J., Tremblay, M.S.
- Physical activity of Canadian children and youth: Accelerometer results from
- the 2007 to 2009 Canadian Health Measures Survey. *Health Reports*
- 412 (Statistics Canada, Catalogue no. 82-003). 2011; 22(1): 15-23.
- 9. da Silva ICM, van Hees VT, Ramires VV et al. Physical activity levels in
- three Brazilian birth cohorts as assessed with raw triaxial wrist accelerometry.
- 415 *Int J Epidemiol*. 2014;43(6):1959-1968.
- 10. Edwardson CL, Harrington DM, Yates T et al. A cluster randomized
- 417 controlled trial to investigate the effectiveness and cost effectiveness of the
- 418 'Girls Active' intervention: a study protocol. *BMC Public Health* 2015
- 419 15:526. doi: 10.1186/s12889-015-1886-z.
- 420 11. Evenson KR, Catellier DJ, Gill K, Ondrak KS, McMurray RG. Calibration of
- two objective measures of physical activity for children. *J Sports Sci*.
- 422 2008;26:1557–65.
- 423 12. Fairclough SJ, Noonan R, Rowlands AV, van Hees V, Knowles Z, Boddy LM.
- Wear compliance and activity in children wearing wrist and hip mounted
- 425 accelerometers. *Med Sci Sports Exerc*. 2016; 48: 243-253. doi:
- 426 10.1249/MSS.0000000000000771.
- 427 13. Fleiss J. *The Design and Analysis of Clinical Experiments*. New York: John
- 428 Wiley & Sons, 1986, p1-31.
- 429 14. Freedson PS, John D. Comment on "Estimating Activity and Sedentary
- Behaviour from an Accelerometer on the Hip and Wrist". *Med Sci Sports*
- 431 *Exerc.* 2013; 45(5): 962 963

432	15. Guinhouya BC, Samouda H, de Beaufort C. Level of physical activity among
433	children and adolescents in Europe: a review of physical activity assessed
434	objectively by accelerometry. Public Health 2013; 127: 301-311.
435	16. Hildebrand M, Van Hees VT, Hansen BH, Ekelund U. Age-Group
436	Comparability of Raw Accelerometer Output from Wrist- and Hip-Worn
437	Monitors. Med Sci Sport Exerc. 2014; 46(9): 1816-1824. doi: 10.1249/MSS.
438	000000000000289.
439	17. Joint Health Surveys Unit, National Centre for Social Research and University
440	College London Research Department of Epidemiology and Public Health.
441	The Health Survey for England 2008. Volume 1: Physical Activity and Fitness.
442	Leeds, United Kingdom: NHS Information Centre for Health and Social Care;
443	2009. (http://www.hscic.gov.uk/catalogue/PUB00430/heal-surv-phys-acti-fitn-
444	eng-2008-rep-v2.pdf). (Accessed March 31, 2016).
445	18. Katzymarzyk PT, Barreira TV, Broyles ST et al. The International Study of
446	Childhood Obesity, Lifestyle and the Environment (ISCOLE): design and
447	methods. BMC Public Health 2013 13:900. doi: 10.1186/1471-2458-13-900.
448	19. Katzymarzyk PT, Barreira TV, Broyles ST et al. Relationship between
449	lifestyle behaviors and obesity in children ages 9–11: Results from a 12-
450	country study. Obesity 2015; 23:1696-1702. doi: 10.1002/oby.21152
451	20. Keane E, Kearney PM, Perry IJ, Browne GM, Harrington JM. Diet, physical
452	activity, lifestyle behaviours, and prevalence of childhood obesity in Irish
453	children: the Cork Children's Lifestyle Study Protocol. JMIR Res Protoc 2014
454	3(3) e44. doi: 10.2196/resprot.3140

- 21. Kearney PM, Harrington JM, McCarthy VJC, Fitzgerald AP, Perry I. Cohort
- 456 Profile: The Cork and Kerry Diabetes and Heart Disease Study. *Int J*
- 457 *Epidemiol* 2013; 42:1253-1262.
- 458 22. Nilsson A, Ekelund U, Yngve A, Sjostrom M. Assessing physical activity
- among children with accelerometers using different time sampling intervals
- and placements. *Ped Exerc Sci* 2002; 14: 87–96.
- 23. Pate RR, Almeida MJ, McIver KL et al. Validation and calibration of an
- accelerom-eter in preschool children. *Obesity* 2006; 14(11): 2000–2006.
- 24. Puyau MR, Adolph AL, Vohra FA, Butte NF. Validation and calibration of
- physical activity monitors in children. *Obes Res.* 2002; 10(3): 150–7.
- 25. Rowlands, A.V., Olds, T.S., Hillsdon, M. et al. Assessing sedentary behaviour
- with the GENEActiv: Introducing the Sedentary Sphere. *Med Sci Sport Exerc*.
- 467 2014; 46: 1235-1247.
- 26. Rowlands AV, Rennie K, Kozarski R et al. Children's physical activity
- assessed with wrist- and hip-worn accelerometers. *Med Sci Sport Exerc*.
- 470 2014; 46: 2308-2316. DOI: 10.1249/MSS.000000000000365.
- 27. Rowlands AV, Yates T, Davies M, Khunti K, Edwardson CL. Raw
- accelerometer data analysis with GGIR R-package: Does accelerometer brand
- 473 matter? *Med Sci Sport Exerc*. 2016. In press.
- 28. Sherar L, Griew P, Esliger D et al. International children's accelerometry
- database (ICAD): Design and methods. *BMC Public Health* 2011; 11:485. doi:
- 476 10.1186/1471-2458-11-485
- 477 29. Troiano RP, Berrigan D, Dodd KW, Mâsse LC, Tilert T, McDowell M.
- Physical activity in the United States measured by accelerometer. *Med Sci*
- 479 Sport Exerc. 2008; 40: 181-188.

480	30. Troiano, R.P., McClain, J.J., Brychtta, R.J., Chen, K.Y. Evolution of
481	accelerometer methods for physical activity research. Br J Sports Med 2014;
482	48: 1019-1023.
483	31. Trost SG, Pate RR, Sallis JF, et al. Age and gender differences in objectively
484	measured physical activity in youth. Med Sci Sports Exerc. 2002; 34: 350-5.
485	32. van Hees VT, Fang Z, Langford J et al. Auto-calibration of accelerometer data
486	for free-living physical activity assessment using local gravity and
487	temperature: an evaluation on four continents. J Appl Physiol. 2014; 117(7):
488	738-744. doi: 10.1152/japplphysiol.00421.2014.
489	33. van Hees VT, Gorzelniak L, Dean León EC et al. Separating Movement and
490	Gravity Components in an Acceleration Signal and Implications for the
491	Assessment of Human Daily Physical Activity. PLoS ONE. 2013; 8(4):
492	e61691. doi: 10.1371/journal.pone.0061691.
493	34. Wake M, Clifford S, York E et al. Introducing Growing Up in Australia's
494	Child Health CheckPoint: A physical health and biomarkers module for the
495	Longitudinal Study of Australian Children. Fam Matters 2014; 94: 15-23

Figure legends

497

498 Figure 1. Time recorded above each of the intensity thresholds by the hip-worn 499 ActiGraph (very low, low, medium and high MVPA count cut-points) and the wrist-500 worn GENEActiv (100+, 150+, 200+, 250+, 300+, 350+, 400+ mg ENMO 501 thresholds) by epoch (ActiGraph <5 s, 15 s, 60 s; GENEActiv <5s) for the total sample. Boxplot shows the median (dark line), 25th and 75th percentiles (box), lowest 502 503 and highest values within 1.5 times the inter-quartile range (whiskers) and outliers 504 (circles). 505 506 Figure 2. The time recorded above each of the intensity thresholds by the hip-worn 507 ActiGraph (very low (a), low (b), medium (c) and high (d) MVPA count cut-points) 508 and the wrist-worn GENEActiv acceleration threshold by epoch (ActiGraph <5 s, 15 509 s, 60 s; GENEActiv <5s) for each of the optimal pairings in the cross-validation 510 sample. Boxplots show the median (dark line), 25th and 75th percentiles (box), lowest 511 and highest values within 1.5 times the inter-quartile range (whiskers) and outliers 512 (circles). 513 514 Figure 3. Kernel density plots showing the distribution of time recorded above each of 515 the intensity thresholds by the hip-worn ActiGraph and the wrist-worn GENEActiv 516 for each of the optimal pairings (total sample). The columns represent cut-points (left 517 to right: very low, low, medium, high) and the rows represent ActiGraph epochs (top 518 to bottom: <5 s, 15 s, 60 s)

519

520

521

List of Supplemental Digital Content

Supplemental Digital Content 1. Docx

Table 1. Participant characteristics (mean \pm standard deviation (SD))

Study	Valid N	Age (y)	Height (cm)	Mass (kg)
	(boys)			
1	51 (26)	11.3 ± 0.6	148.7 ± 6.8	44.1 ± 11.2
2	108 (42)	10.0 ± 0.3	139.1 ± 7.6	35.4 ± 8.5
1 & 2 (Test sample)	159 (68)	10.4 ± 0.7	142.2 ± 8.6	38.3 ± 10.3
3 (Cross-validation sample)	79 (5)	10.3 ± 0.6	142.1 ± 7.8	36.9 ± 8.6
Total sample	238 (103)	10.4 ± 0.7	142.2 ± 8.3	37.8 ± 9.7

Table 2. Agreement between each hip-worn ActiGraph cut-point and each wrist-worn GENEActiv ENMO threshold by epoch length in the test sample (N=159)

HIP	WRIST	Ac	ActiGraph ≤5 s epoch			Graph 15 s epoc	h	ActiGraph 60 s epoch		
ActiGraph cut-point	GENEActiv ENMO ^e (mg)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)
Very low ^a	100+	0.29 (-0.09, 0.62)	55.9	59.6	0.43 (-0.10, 0.72)	42.8	58.7	0.47 (-0.08, 0.75)	40.7	61.6
	150+	0.71 (0.62, 0.78)	-2.9	43.9	0.67 (0.33, 0.82)	-15.9	44.1	0.65 (0.31, 0.81)	-18.0	49.5
	200+	0.36 (-0.10, 0.69)	-34.6	39.6	0.30 (-0.08, 0.65)	-47.7	41.8	0.31 (-0.09, 0.65)	-49.8	49.4
	250+	0.18 (-0.06, 0.49)	-53.0	39.4	0.16 (-0.05, 0.46)	-66.0	43.4	0.18 (-0.06, 0.48)	-68.1	52.2
	300+	0.11 (-0.04, 0.36)	-64.3	40.0	0.10 (-0.04, 0.35)	-77.3	45.3	0.12 (-0.05, 0.37)	-79.4	54.9
	350+	0.08	-71.8	40.8	0.08 (-0.03, 0.28)	-84.9	47.1	0.09 (-0.04, 0.30)	-87.0	57.1
	400+	0.06 (-0.03, 0.23)	-77.2	41.7	0.06 (-0.03, 0.23)	-90.3	48.7	0.07 (-0.04, 0.24)	-92.4	59.0
Low ^b	100+	0.16 (-0.06, 0.44)	80.4	61.6	0.18 (-0.06, 0.49)	79.8	60.9	0.17 (-0.06, 0.47)	86.4	63.0
	150+	0.53 (0.01, 0.77)	21.6	41.2	0.59 (0.05, 0.81)	21.0	40.6	0.53 (-0.07, 0.79)	27.6	42.7
	200+	0.67 (0.41, 0.80)	-10.1	32.7	0.71 (0.44, 0.83)	-10.7	33.5	0.75 (0.67, 0.81)	-4.1	36.4
	250+	0.37 (-0.09, 0.70)	-28.5	30.1	0.41 (-0.10, 0.73)	-29.1	32.5	0.51 (-0.06, 0.77)	-22.5	36.1
	300+	0.22 (-0.06, 0.55)	-39.8	29.6	0.25 (-0.07, 0.59)	-40.4	33.3	0.33 (-0.10, 0.66)	-33.8	37.5
	350+	0.15 (-0.04, 0.44)	-47.3	29.9	0.18 (-0.06, 0.49)	-47.9	34.5	0.23 (-0.08, 0.56)	-41.3	39.0

	400+	0.11	-52.7	30.6	0.13	-53.3	35.9	0.18	-46.7	40.5
		(-0.04, 0.36)			(-0.05, 0.41)			(-0.07, 0.47)		
Medium ^c	100+	0.09 (-0.04, 0.29)	101.6	65.9	0.09 (-0.04, 0.31)	105.8	65.5	0.08 (-0.04, 0.28)	115.2	66.9
	150+	0.26 (-0.09, 0.59)	42.8	43.1	0.27 (-0.08, 0.60)	47.1	42.2	0.21 (-0.06, 0.54)	56.4	43.3
	200+	0.63 (0.30, 0.79)	11.1	31.7	0.61 (0.09, 0.82)	15.3	31.1	0.48 (-0.10, 0.77)	24.7	32.0
	250+	0.69 (0.48, 0.80)	-7.3	26.4	0.76 (0.69, 0.82)	-3.0	26.7	0.73 (0.59, 0.82)	6.4	27.7
	300+	0.46 (-0.10, 0.76)	-18.6	24.3	0.58 (0.00, 0.81)	-14.4	25.6	0.73 (0.61, 0.81)	-5.0	26.6
	350+	0.30 (-0.08, 0.65)	-26.1	23.6	0.41 (-0.10, 0.73)	-21.9	25.7	0.58 (0.10, 0.79)	-12.5	26.9
	400+	0.22 (-0.06, 0.55)	-31.5	23.6	0.30 (-0.08, 0.64)	-27.3	26.4	0.45 (-0.08, 0.73)	-17.9	27.6
High ^d	100+	0.05 (-0.03, 0.17)	122.0	71.3	0.04 (-0.03, 0.16)	130.4	72.1	0.03 (-0.02, 0.13)	139.5	73.9
	150+	0.12 (-0.05, 0.37)	63.3	47.1	0.10 (-0.05, 0.33)	71.7	47.8	0.07 (-0.04, 0.27)	80.7	49.6
	200+	0.28 (-0.09, 0.61)	31.6	33.4	0.21 (-0.07, 0.54)	40.0	34.1	0.15 (-0.05, 0.43)	49.0	35.6
	250+	0.54 (0.03, 0.77)	13.2	25.7	0.40 (-0.10, 0.71)	21.6	27.3	0.26 (-0.08, 0.59)	30.7	27.6
	300+	0.73 (0.65, 0.80)	1.8	21.5	0.60 (0.12, 0.80)	10.3	22.3	0.40 (-0.10, 0.71)	19.3	23.2
	350+	0.69 (0.46, 0.81)	-5.7	19.3	0.73 (0.64, 0.80)	2.7	20.2	0.54 (-0.02, 0.78)	11.8	20.8
	400+	0.55 (-0.04, 0.80)	-11.1	18.3	0.72 (0.64, 0.80)	-2.6	19.2	0.65 (0.36, 0.79)	6.5	19.5

^aVery low = 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31) = 1680 cpm, Pate et al. (23)

528	^c Medium	= 2296 cpm, Evenson et al. (11)
529	^d High	= 3200 cpm, Puyau et al. (24)
530	^e ENMO	= Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity
531	fICC	= Intra-class correlation coefficient
532	^g 95% CI	= 95% confidence interval
533	$^{\rm h}{ m LoA}$	= Limits of agreement
534	The ENMO t	hreshold with the highest agreement for each ActiGraph count cut-point / epoch combination is highlighted in bold.

Table 3. Cross-validation sample: Agreement between the hip-worn ActiGraph and wrist-worn GENEActiv for the optimal ENMO threshold for each ActiGraph count cut-point / epoch combination (N = 79)

	GENEActiv	Act	iGraph ≤5 s epoc	ch	ActiGr	raph 15 s epoch		ActiGra	aph 60 s epoc	h
ActiGraph cut-point HIP	ENMO ^e (mg) WRIST	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)
Very low ^a	150+	0.63 (0.46, 0.75)	7.0	39.4	0.71 (0.57, 0.80)	-5.9	39.1	0.69 (0.55, 0.80)	-6.2	42.6
Low ^b	200+	0.66 (0.51, 0.77)	-3.8	31.0	0.71 (0.58, 0.80)	-3.0	31.2	0.69 (0.55, 0.80)	5.3	32.8
Medium ^c	250+	0.64 (0.49, 0.76)	-3.6	25.7	0.70 (0.57, 0.80)	2.0	13.1			
	300+							0.69 (0.56, 0.79)	2.2	23.8
High ^d	300+	0.62 (0.46, 0.74)	2.7	21.5						
	350+				0.61 (0.33, 0.76)	5.5	18.7			
	400+							0.42 (-0.04, 0.69)	9.7	18.2

540

541

542

543

544

547

536

537

aVery low = 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31)

^bLow = 1680 cpm, Pate et al. (23)

= 2296 cpm, Evenson et al. (11) ^cMedium

= 3200 cpm, Puyau et al. (24) ^dHigh **eENMO**

= Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity

^fICC = Intra-class correlation coefficient

= 95% confidence interval 545 ^g95% CI 546

 ^{h}LoA = Limits of agreement Supplementary Table. Agreement between each hip-worn ActiGraph cut-point and each wrist-worn GENEActiv ENMO threshold by epoch length in the total sample (N = 238)

HIP	WRIST	Act	ActiGraph ≤5 s epoch			ActiGraph 15 s epoch			ActiGraph 60 s epoch		
ActiGraph cut-point	GENEActiv ENMO ^e (mg)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^g (+/- min)	ICC ^f (95% CI ^g)	Mean bias (G-AG, min)	95% LoA ^h (+/- min)	
Very low ^a	100+	0.27 (-0.09, 0.60)	57.5	59.6	0.36 (-0.10, 0.68)	44.5	57.1	0.44 (-0.09, 0.73)	43.0	59.6	
	150+	0.70 (0.63, 0.76)	0.4	43.4	0.68 (0.57, 0.76)	-12.6	43.4	0.67 (0.45, 0.79)	-14.1	48.5	
	200+	0.39 (-0.10, 0.70)	-30.5	38.6	0.34 (-0.10, 0.66)	-43.5	40.9	0.33 (-0.09, 0.66)	-45.0	48.0	
	250+	0.19 (-0.06, 0.51)	-48.4	38.0	0.18 (-0.06, 0.48)	-61.4	42.2	0.18 (-0.06, 0.49)	-62.9	50.4	
	300+	0.12 (-0.04, 0.39)	-59.4	38.5	0.12 (-0.05, 0.37)	-72.4	44.0	0.12 (-0.05, 0.37)	-73.9	52.8	
	350+	0.09	-66.8	39.3	0.08	-79.8	45.7	0.09	-81.3	54.8	
	400+	(-0.04, 0.29) 0.064 (-0.03, 0.24)	-72.0	40.2	(-0.04, 0.29) 0.07 (-0.04, 0.24)	-85.0	47.3	(-0.04, 0.30) 0.07 (-0.04, 0.25)	-86.5	56.6	
Low ^b	100+	0.15 (-0.06, 0.43)	79.9	80.0	0.16 (-0.06, 0.46)	79.9	59.5	0.16 (-0.05, 0.45)	87.1	61.1	
	150+	0.50 (-0.02, 0.75)	22.9	41.1	0.54 (-0.01, 0.78)	22.8	40.5	0.48 (-0.09, 0.76)	29.9	42.6	
	200+	0.68 (0.51, 0.78)	-8.0	32.7	0.71 (0.54, 0.80)	-8.2	33.4	0.74 (0.68, 0.80)	-1.0	36.3	
	250+	0.39 (-0.10, 0.71)	-25.9	29.7	0.42 (-0.10, 0.73)	-26.0	32.1	0.54 (0.01, 0.77)	-18.9	35.6	
	300+	0.23 (-0.06, 0.56)	-36.9	29.0	0.25 (-0.07, 0.59)	-37.1	32.6	0.35 (-0.10, 0.67)	-29.9	36.6	
	350+	0.15 (-0.05, 0.45)	-44.3	29.2	0.18 (-0.06, 0.48)	-44.4	33.7	0.25 (-0.09, 0.57)	-37.3	37.9	

	400+	0.11	-49.5	29.7	0.13	-49.7	34.9	0.19	-42.5	39.3
		(-0.04, 0.37)			(-0.05, 0.40)			(-0.08, 0.49)		
Medium ^c	100+	0.08 (-0.04, 0.28)	99.9	66.1	0.08 (-0.04, 0.29)	104.6	64.0	0.07 (-0.03, 0.26)	114.4	65.5
	150+	0.25 (-0.09, 0.57)	42.8	42.9	0.25 (-0.08, 0.58)	47.4	42.1	0.19 (-0.06, 0.51)	57.3	43.4
	200+	0.60 (0.25, 0.77)	11.8	31.7	0.59 (0.10, 0.79)	16.5	33.4	0.43 (-0.10, 0.74)	26.3	32.5
	250+	0.68 (0.53, 0.78)	-6.1	26.4	0.74 (0.67, 0.79)	-1.4	26.7	0.69 (0.45, 0.81)	8.5	27.9
	300+	0.47 (-0.09, 0.75)	-17.1	24.0	0.55 (-0.02, 0.79)	-12.4	25.3	0.73 (0.66, 0.78)	-2.6	26.5
	350+	0.31 (-0.08, 0.65)	-24.5	23.2	0.38 (0.10, 0.71)	-19.8	25.2	0.61 (0.25, 0.78)	-9.9	26.5
	400+	0.22 (-0.06, 0.55)	-29.7	23.1	0.28 (-0.08, 0.61)	-24.9	25.7	0.48 (-0.03, 0.73)	-15.2	27.0
High ^d	100+	0.04 (-0.03, 0.17)	119.1	71.4	0.04 (-0.03, 0.15)	128.0	70.5	0.03 (-0.02, 0.12)	137.1	72.7
	150+	0.11 (-0.05, 0.36)	62.0	46.5	0.10 (-0.05, 0.31)	70.9	47.3	0.07 (-0.04, 0.24)	79.9	49.5
	200+	0.26 (-0.09, 0.58)	31.1	33.3	0.21 (-0.08, 0.52)	39.9	33.4	0.13 (-0.05, 0.40)	49.0	36.0
	250+	0.51 (0.02, 0.75)	13.2	25.7	0.40 (-0.09, 0.69)	22.1	26.3	0.23 (-0.08, 0.55)	31.1	28.0
	300+	0.71 (0.64, 0.77)	2.1	21.5	0.60 (0.30, 0.76)	11.0	22.1	0.35 (-0.10, 0.67)	20.1	23.4
	350+	0.68 (0.48, 0.79)	-5.2	19.2	0.70 (0.63, 0.76)	3.7	19.9	0.48 (-0.06, 0.75)	12.7	20.8
	400+	0.54 (-0.03, 0.78)	-10.5	18.1	0.65 (0.48, 0.76)	-1.6	18.7	0.59 (0.22, 0.36)	7.5	19.3

aVery low = 1100 cpm, approximately equivalent to the 3 MET cut-point, age 11 y, age-specific criteria of the Freedson group, published by Trost et al. (31) = 1680 cpm, Pate et al. (23)

552	^c Medium	= 2296 cpm, Evenson et al. (11)				
553	^d High	= 3200 cpm, Puyau et al. (24)				
554	^e ENMO	= Euclidean Norm Minus One, the vector magnitude of acceleration corrected for gravity				
555	fICC	= Intra-class correlation coefficient				
556	^g 95% CI	= 95% confidence interval				
557	$^{\rm h}{ m LoA}$	= Limits of agreement				
558	The ENMO threshold with the highest agreement for each ActiGraph count cut-point / epoch combination in the test sample is highlighted in bold					
559						
560						





