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2

3 *Title: Comparison of children's free-living physical activity derived from wrist and hip raw*
4 *accelerations during the segmented week.*

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22

Abstract

23 This study assessed children's physical activity (PA) levels derived from wrist-worn GENEActiv and
24 hip-worn ActiGraph GT3X+ accelerometers and examined the comparability of PA levels between the
25 two devices throughout the segmented week. One hundred twenty nine 9-10 year old children (79 girls)
26 wore a GENEActiv (GAwrist) and ActiGraph GT3X+ (AGhip) accelerometer on the left wrist and right
27 hip respectively for seven days. Mean minutes of light PA (LPA) and moderate-to-vigorous PA
28 (MVPA) per weekday (whole-day, before-school, school and after-school) and weekend day (whole-
29 day, morning and afternoon-evening) segments were calculated, and expressed as percentage of
30 segment time. Repeated measures ANOVA examined differences in LPA and MVPA between GAwrist
31 and AGhip for each time segment. Bland–Altman plots assessed between-device agreement for LPA
32 and MVPA for whole weekday and whole weekend day segments. Correlations between GAwrist and
33 AGhip were weak for LPA ($r=0.18-0.28$), but strong for MVPA ($r=0.80-0.86$). LPA and MVPA levels
34 during all weekday and weekend day segments were significantly higher for GAwrist than AGhip
35 ($p<0.001$). The largest inter-device percent difference of 26% was observed in LPA during the school
36 day segment. Our data suggest that correction factors are needed to improve raw PA level comparability
37 between GAwrist and AGhip.

38

39

Introduction

40 Accelerometers provide valid and reliable assessments of physical activity (PA) at varying intensities
41 in children (Butte, Ekelund, & Westerterp, 2012; de Vries et al., 2009), and are the most widely used
42 objective measure of child PA (Cain, Sallis, Conway, Van Dyck, & Calhoun, 2013). One of the
43 advantages of using accelerometers is their ability to capture PA variability within and between days.
44 Accelerometer device output is traditionally expressed as an arbitrary 'count' value which is then related
45 to specific PA intensity thresholds. Due to differences in how raw data are processed, filtered, and
46 scaled, count data cannot be directly compared across studies using different accelerometer devices
47 (Welk, McClain, & Ainsworth, 2012). However, the latest versions of accelerometers, including

48 GENEActiv and ActiGraph GT3X+ can provide raw, unfiltered acceleration data. Compared to
49 traditional count-based approaches, raw acceleration data offers greater control over data reduction,
50 potentially allowing comparisons to be made more easily between studies using different accelerometer
51 brands (Fairclough et al., 2016; Hildebrand, Van Hees, Hansen, & Ekelund, 2014).

52 Aside from the challenge of comparing PA levels between device brands, another challenge is the
53 comparability of PA levels between devices placed at different body locations. Traditionally,
54 accelerometers are worn at the hip to capture whole-body movement, but compliance to device wear is
55 typically low (Fairclough et al., 2016). In an attempt to improve device wear there has been an increased
56 use of wrist-worn accelerometers, including the GENEActiv. Compared to hip-worn accelerometers,
57 wrist-worn accelerometers are more sensitive to upper body movement (e.g. climbing, throwing) but
58 less sensitive to sedentary activities (Ellis et al., 2014; Ellis, Kerr, Godbole, Staudenmayer, & Lanckriet,
59 2016; Kim, Lee, Peters, Gaesser, & Welk, 2014). This may limit the comparison of findings between
60 studies using wrist and hip-worn accelerometers. Given the increased use of the wrist-worn GENEActiv
61 (da Silva et al., 2014; Edwardson et al., 2015; Keane, Kearney, Perry, Browne, & Harrington, 2014;
62 Wake et al., 2014), and the wealth of existing international data obtained from hip-worn ActiGraph
63 accelerometers (Cooper et al., 2015; Corder et al., 2016; Sherar et al., 2011) it is important to understand
64 whether PA estimates derived from GA_{wrist} and AG_{hip} are comparable.

65 Fairclough et al. (2016) compared children's whole-day MPA and VPA derived from the GA_{wrist} and
66 AG_{hip} and found that mean PA levels for both intensities were significantly higher for the GA_{wrist}
67 than the AG_{hip}. However, the comparability of PA levels between the GA_{wrist} and AG_{hip} at the lower
68 end of the intensity spectrum is less well understood. Moreover, the agreement between the GA_{wrist}
69 and AG_{hip} may fluctuate in response to variability in PA levels both within and between days (Brooke,
70 Corder, Atkin, & van Sluijs, 2014; Fairclough, Beighle, Erwin, & Ridgers, 2012). However, studies
71 comparing GA_{wrist} and AG_{hip} data have been limited to reporting PA estimates (Fairclough et al.,
72 2016; Rowlands et al., 2014), and raw accelerations across the whole day (Rowlands et al., 2015).
73 Therefore, little is known about their comparability across specific time-segments. For that reason, the

74 aim of this study was to assess children's PA levels derived from GA_{wrist} and AG_{hip} raw acceleration
75 data, and examine the comparability of PA levels between the two devices throughout the segmented
76 week.

77 **Methods**

78 *Participants and settings*

79 The participants were 129 children (79 girls) aged 9-10 years (age: 10.1 ± 0.3 y (mean \pm SD)) from six
80 schools in Liverpool, England. After ethical approval from the university research ethics committee
81 (13/SPS/048), all year 5 children (n = 326) in participating schools were invited to participate and
82 received parent and child information sheets, and consent and assent forms, to take home to parents and
83 return upon completion. Written informed consent and assent were received from parents and their
84 children, respectively, before children could participate in the study. Data collection took place between
85 January and May 2014.

86 *Procedure and measurements*

87 Each child wore a GENEActiv (GA_{wrist}; Activinsights, Cambs, UK) and ActiGraph GT3X+ (AG_{hip};
88 ActiGraph, Pensacola, FL) accelerometer on their left wrist and right hip, respectively, for seven
89 consecutive days. The GA_{wrist} was selected because it measures raw accelerations, is typically worn
90 on the wrist, and has demonstrated reliability and validity in child populations (Phillips, Parfitt, &
91 Rowlands, 2013). ActiGraph accelerometers are the most commonly used accelerometer in child PA
92 research (Cain et al., 2013). The GT3X+ model was selected because it is traditionally worn on the hip
93 (Rosenberger et al., 2013), has the capability to generate raw acceleration, and has been validated for
94 use with children (Hanggia, Phillips, & Rowlands, 2013; Robusto & Trost, 2012). Children were
95 instructed to wear both monitors concurrently during all waking hours except when engaged in water-
96 based activities. Verbal and written instructions for care and placement of the monitors were given to
97 children. Prior to testing, monitors were synchronised with Greenwich Mean Time (GMT) and

98 programmed to record data at 100 Hz. Data collection took place during the regular school term so
99 activities were representative of usual free-living activities.

100 *Data analysis*

101 GAWrist data were downloaded using GENEActiv v.2.2 software (Activinsights, Cambs, UK) and
102 saved in raw format as binary files. AGhip data were downloaded using ActiLife v. 6.11.4 (ActiGraph,
103 Pensacola, FL) and saved in raw format as GT3X files. These were subsequently converted to CSV
104 format to facilitate raw data processing. GAWrist and AGhip raw data files were then processed in R
105 (<http://cran.r-project.org>) using the GGIR package (version 1.1-4) which converted raw triaxial
106 acceleration values into one omnidirectional measure of acceleration, termed the signal vector
107 magnitude (SVM). SVM was calculated from raw accelerations from the three axes minus 1g which
108 represents the value of gravity (i.e., $SVM = \sqrt{(x^2 + y^2 + z^2)} - 1$), after which negative values were
109 rounded to zero. This metric is referred to as the Euclidean norm minus one (ENMO) (van Hees et al.,
110 2013). Raw data were further reduced by calculating the average SVM values per 1-s epoch expressed
111 in *mg* over each of the 7 monitored days. Wear time periods for raw data from GAWrist and AGhip
112 were estimated on the basis of the standard deviation and value range of each axis, calculated for 60
113 min moving windows with 15 min increments (van Hees et al., 2013). A time window was classified as
114 non-wear time if, for at least 2 out of the 3 axes, the standard deviation was less than 13.0 *mg* or if the
115 value range was less than 50 *mg* (van Hees et al., 2013). A valid day was classified as 10 hours or more
116 of device wear. At a minimum, children were required to have worn both devices on the same 3 days
117 including 1 weekend day to be included in the analyses. (Mattocks et al., 2008).

118 We used device specific prediction equations provided by Hildebrand et al. (2014) to identify ENMO
119 cut-points for classifying LPA and MVPA (Hildebrand et al., 2014). It has recently been reported that
120 in youth 2 METs and 4 METs had higher classification accuracy for differentiating sedentary time (from
121 LPA) and MVPA (from LPA), respectively, compared with 1.5 METs and 3 METs (Saint-Maurice,
122 Kim, Welk, & Gaesser, 2016). Therefore, the Hildebrand equations were solved for 2 METs and 4
123 METs resulting in LPA and MPVA cut-points of 23.5*mg* and 359.7*mg*, respectively, for GAWrist, and

124 35.2mg and 249.9mg, respectively, for AGhip. For example, the GAwrist LPA mg cut-point threshold
125 was calculated as follows: $mg = ((2METs \times 6 \text{ mL O}_2 \cdot \text{kg}^{-1} \cdot \text{min}^{-1}) - 11.16) / 0.0357 = 23.5mg$.

126 Once converted to minutes of LPA and MVPA, data were sorted into hourly segments from 06:30 until
127 23:59 on weekdays and weekend days using Stata (STATA/SE Version 12; StataCorp LP, College
128 Station, TX) code developed by the third author. Sleep time was defined as midnight until 06:30. These
129 hourly values were then used to construct whole-day and segmented day minutes of LPA and MVPA.
130 During weekdays the following time segments were used: before-school (06.30 to 08:59), during school
131 (09:00 to 15:29), and after-school (15:30 to 23:59). For weekend days the segments were: morning
132 (06:30 to 11:59) and afternoon-evening (12:00 to 23:59). Variables were calculated by summing
133 minutes spent in each activity threshold during each discrete time segment. Mean minutes of GAwrist
134 and AGhip LPA and MVPA data for each segment were divided by total segment time, multiplied by
135 100, and expressed as percentage of total segment time.

136 The primary outcome variables were percentage segment time for LPA and MVPA. Repeated measures
137 ANOVAs examined between segment differences for each device (e.g., GAwrist LPA whole weekday
138 vs GAwrist LPA whole weekend day), and between device differences for each segment (e.g., GAwrist
139 LPA whole weekday vs AGhip LPA whole weekend day). Pearson correlation analyses examined
140 associations between the two devices for percentage of time spent in LPA and MVPA during whole-
141 day weekday and weekend day. Bland–Altman plots were constructed to assess between-device
142 agreement of LPA and MVPA for whole weekday and whole weekend day segments. All analyses were
143 conducted using IBM SPSS Statistics v.23 (IBM, Armonk, NY) and Microsoft Excel 2010 (Microsoft,
144 Redmond, WA). For all analyses, statistical significance was set at 0.05.

145 **Results**

146 AGhip and GAwrist data were available for 115 and 128 children, respectively. Participants not meeting
147 the wear time criteria for either monitor were excluded from analyses. This reduced the sample to 107
148 (67 girls) for the GAwrist and 83 (51 girls) for the AGhip. Children without 3 valid days for both

149 monitors were then excluded from the analysis, resulting in a final analytical sample of 77 (48 girls)
150 participants. There were no significant differences for any of the measured variables between children
151 included in analyses and those excluded. Means and 95% confidence intervals (CI) for PA outcomes
152 on weekdays and weekend days for GA wrist and AG hip are presented in Table 1. Whole weekday PA
153 outcomes were higher than mean whole weekend day PA outcomes ($p<0.05$). PA outcomes were higher
154 during the school segment compared to all other weekday segments ($p<0.001$). On weekend days
155 children were more active in the afternoon-evening compared to the morning ($p<0.01$).

156 GA wrist PA levels were significantly higher than AG hip PA levels during all weekday and weekend
157 day segments ($p<0.001$; Table 1) but varied between time segments and PA intensities. On weekdays
158 the largest inter-device differences in PA levels occurred during the school segment (LPA 26.7%;
159 MVPA 1.8%; $p<0.001$), and the smallest inter-device differences occurred in the before school segment
160 (LPA 10.3%; MVPA 0.5%; $p<0.001$). On weekend days the largest inter-device differences occurred
161 in the afternoon-evening (LPA 17.7%; MVPA 1.6%; $p<0.001$), and the smallest inter-device differences
162 occurred in the morning (LPA 10.3%, MVPA 0.8%; $p<0.001$). For all intensities the magnitude of inter-
163 device differences was largest at weekends compared to weekdays.

164 Significant correlations between whole weekday ($r=0.80$) and whole weekend day ($r=0.86$) MVPA
165 levels confirmed that MVPA was strongly associated between devices ($p<0.001$). Correlations between
166 the devices were weak for LPA during whole weekdays ($r=0.28$ $p<0.01$) and whole weekend days
167 ($r=0.18$; $p=0.11$). Bland–Altman plots (Figure 1) show the extent of differences in LPA and MVPA
168 between GA wrist and AG hip during whole weekdays and weekend days.

169 [TABLE 1 NEAR HERE]

170 [FIGURE 1 NEAR HERE]

171 **Discussion**

172 This is the first study to compare children's LPA and MVPA assessed with GA wrist and AG hip across

173 distinct time windows in a week. Another novel aspect of this study is the use of raw data processing
174 techniques, which theoretically enables direct comparisons of activity outcomes obtained from different
175 accelerometer brands. Overall, we observed weak correlations between AGhip and GAwrist for LPA
176 ($r=0.18-0.28$), but strong correlations for MVPA ($r=0.80-0.86$). The strong correlations observed for
177 MVPA are similar to those reported by Fairclough et al. (2016). They are though slightly lower than
178 the reported correlation of $r=0.93$ between hip-worn GENEActiv and ActiGraph GT3X+ mean
179 accelerations (Rowlands et al., 2015). Despite these strong associations, we found that GAwrist derived
180 PA levels were consistently higher than those derived from the AGhip for all outcome variables and
181 across various time segments. These findings suggest that child PA surveillance is strongly influenced
182 by device brand and body placement.

183 LPA and MVPA levels during all weekday and weekend day segments were significantly higher for the
184 GAwrist than those for the AGhip ($p<0.001$). Previous research comparing whole-day accelerometer
185 output from wrist-worn GENEActiv and hip-worn ActiGraph in children reported similar findings
186 (Fairclough et al., 2016; Hildebrand et al., 2014). Fairclough et al. (2016) reported a 68% difference in
187 the number of children achieving at least 60 minutes of MVPA per day using the GENEActiv compared
188 to ActiGraph GT3X+. Similarly, Rowlands et al. (2015) found that average daily accelerations from the
189 wrist-worn GENEActiv were between 12%–13% higher than the ActiGraph GT3X+. Another recent study
190 found that the ActiGraph GT3X+ worn on the wrist produced higher average step counts per day
191 compared to the ActiGraph GT3X+ at the hip in free-living environments, but fewer steps during
192 laboratory treadmill testing (Tudor-Locke, Barreira, & Schuna, 2015). These contrasting differences in
193 step outputs between research settings are likely consequential of the restrictive nature of treadmill
194 walking which minimises free swinging of the arms relative to free-living.

195 A unique element of this study is the comparison of PA levels between GAwrist and AGhip across
196 different time segments. We found that differences in PA levels between the two devices varied in
197 magnitude between intensity levels. As the intensity level increased, the magnitude of the difference in
198 PA levels between the GAwrist and AGhip decreased. The largest differences in PA levels were seen

199 in LPA. . Mean GA_{wrist} LPA was over 100% higher than that for the AG_{hip} in all segments with the
200 exception of the before school segment.

201 During free-living children typically engage in a range of seated activities that involve a high level of
202 arm movement but limited movement at the hip (Kim et al., 2014). Unsurprisingly, during such
203 activities, disproportionate levels of acceleration will be observed at the wrist relative to the hip. This
204 is reflected by the high inter-device difference in LPA during the school day segment. LPA accounted
205 for 42.6% and 15.6% of school segment time for the GA_{wrist} and AG_{hip}, respectively, a difference of
206 over 26%. The profound difference in LPA observed during the school day likely reflects these
207 disjointed wrist and hip movement patterns when children characteristically spend a large proportion of
208 the day seated at a desk reading, writing, or using a computer which all involve some element of wrist
209 movement. Greater accelerations will also be observed at the wrist relative to the hip during mixed
210 static/dynamic movements (e.g., playing catch), and high intensity activities such as running and
211 jumping that naturally incur a medium to high level of shoulder and upper body rotation (Ellis et al.,
212 2014, 2016; Kim et al., 2014). However, the level of decoupling (i.e., greater acceleration capture at
213 one wear site relative to the other) during such activities is likely dependent on individual biomechanics
214 (i.e., level of arm swing), and thus will be population specific (Rowlands & Stiles, 2012; Tudor-Locke
215 et al., 2015).

216 The weaker correlations and larger inter-device differences observed for LPA compared to MVPA
217 suggests that in children of this age, pro-wrist “decoupling”, is more dominant during LPA. In contrast,
218 earlier studies observed greater decoupling as the magnitude of acceleration increased. However, these
219 studies did not examine accelerations at intensities lower than 3 METs (Fairclough et al., 2016;
220 Hildebrand et al., 2014). Children’s free-living accelerations were over 10% greater for the GENEActiv
221 compared to the ActiGraph in a recent study when both devices were worn at the hip (Rowlands et al.,
222 2015). This suggests that additional factors other than monitor placement may have also contributed to
223 the observed differences in GA_{wrist} and AG_{hip} PA levels. Similarly, John, Sasaki, and Staudenmayer
224 (2013) found that GENEActiv peak accelerations were up to 7.4% greater than ActiGraph peak

225 accelerations during mechanical shaker testing. Irrespective of placement location, potential factors that
226 may cause inter-monitor differences in raw acceleration between the GAWrist and AGhip include
227 differences in microelectromechanical sensors, dynamic ranges and proprietary filtering processes used
228 to minimise signal distortion during initial analogue-to-digital conversion (John & Freedson, 2012; John
229 et al., 2013). Therefore, the current generation of accelerometry-based monitors may not be directly
230 compared with each other even at the raw acceleration level, due to the discrepancies in how the raw
231 data are collected and filtered. Further research and/or discussions are required to achieve the “true”
232 harmonization of raw data collected from different types of devices.

233 A common outcome in child PA research is time spent in MVPA which is used to identify the number
234 of children meeting the PA guidelines (i.e. at least 60 min of MVPA per day) (Chief Medical Officers,
235 2011). To complicate comparisons further between GAWrist and AGhip, accelerometer data are
236 commonly analysed using a broad range of intensity thresholds leading to widely varying estimates of
237 MVPA within and between studies (Guinhouya, Samouda, & de Beaufort, 2013; Routen, Upton,
238 Edwards, & Peters, 2012). For example, Schaefer, Nace, and Browning (2014) found that estimates of
239 wrist derived MVPA decreased by 27% (from 308 to 225 minutes) when the MVPA cut-point threshold
240 was increased from 3 METs to 4 METs. The difference in MVPA levels between GAWrist and AGhip
241 within this study and between other studies highlights the influence of device and wear location on
242 MVPA prevalence, and the challenge of comparing MVPA data between studies using different
243 intensity thresholds and devices worn at different body locations. Rowlands et al. (2015) found that
244 applying a population specific correction factor to the GAWrist data removed the significant difference
245 in accelerations between GAWrist and AGhip data. This method may therefore be an appropriate way
246 of improving the comparability of findings between studies using different device brands and placement
247 locations in the future.

248 This is the first study to examine the comparability of GAWrist and AGhip derived LPA and MVPA
249 throughout the segmented week. The study observed differential agreement between GAWrist and
250 AGhip. Agreement differed according to PA intensity and time of day, with the greatest difference

251 occurring in LPA during school hours. Future studies should therefore be cautious when comparing PA
252 data derived from GAwrist and AGhip, especially studies investigating children’s school day PA and
253 segmented days. PA levels were derived from raw acceleration data and were processed and analysed
254 using the same open-source procedures, which adds transparency and consistency to the data. However,
255 the results of this study were performed in a relatively small sample of children living in a highly
256 deprived area of England, which limits the generalisability of findings to other locations and
257 populations. Device wear time was greater for the GAwrist compared to the AGhip which may have
258 contributed to the observed differences in PA levels. The inclusion criteria used in this study for whole-
259 day device wear is consistent with recommendations and common practices, but we did not apply wear
260 time criteria to specific time segments (e.g., before-school). This may have biased the PA outcomes for
261 individual segments depending on segment wear time.

262 **Conclusion**

263 In conclusion, PA levels from the GAwrist and AGhip are not comparable under free-living conditions.
264 PA levels derived using raw data processing procedures were significantly higher for GAwrist
265 compared with those for AGhip during all time segments. The magnitude of these differences was
266 greatest during school hours and in LPA. Comparisons of raw data assessed by different monitors worn
267 at the wrist and hip in children should therefore be undertaken with caution. We recommend the
268 development of PA level correction factors to aid comparison of findings between studies using the
269 GAwrist and AGhip.

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Table 1 Physical activity outcomes for GAwrst and AGhip for weekday and weekend day segments

	GAwrst			AGhip			GAwrst - AGhip segment difference		
	Mean minutes	95% CI	% segment time	95% CI	Mean minutes	95% CI	% segment time	95% CI	%
LPA									
Whole week	306.8	291.3 - 322.3	29.2	27.9 - 30.9	128.8	118.3 - 139.5	12.3	11.3 - 13.4	16.9***
Whole weekday	329.9	316.6 - 343.3	31.5+++	30.3 - 33.0	134.7	124.4 - 145.1	12.9+	11.8 - 13.9	18.6***
Before school	34.8	31.6 - 38.0	23.3	21.1 - 25.6	18.3	16.0 - 20.5	12.3	10.8 - 13.8	11.0***
During school	165.5	160.1 - 173.0	42.6‡‡‡	40.6 - 44.5	61.7	56.4 - 67.4	15.9‡‡‡	14.6 - 17.3	26.7***
After school	129.6	121.7 - 137.5	25.5	23.7 - 27.2	54.7	49.3 - 60.1	10.8	9.8 - 11.9	14.7***
Whole weekend day	283.6	265.9 - 301.3	27.1	25.4 - 28.8	122.9	112.1 - 133.8	11.7	10.7 - 12.8	15.4***
Morning	58.3	48.4 - 68.1	17.7	14.7 - 20.7	24.5	20.5 - 28.6	7.4	6.2 - 8.7	10.3***
Afternoon-evening	225.4	213.0 - 37.8	31.4†††	29.6 - 33.1	98.3	88.5 - 108.2	13.7†††	12.3 - 15.1	17.7***
MVPA									
Whole week	30.0	27.3 - 32.8	2.9	2.6 - 3.2	16.5	14.5 - 18.5	1.6	1.4 - 1.8	1.3***
Whole weekday	31.9	29.7 - 34.2	3.0+	2.8 - 3.3	18.7	17.2 - 20.2	1.8+++	1.7 - 2.0	1.2***
Before school	2.4	2.0 - 2.8	1.6	1.4 - 1.9	1.7	1.4 - 2.0	1.1	0.9 - 1.3	0.5***
During school	16.7	15.3 - 18.0	4.3‡‡‡	3.9 - 4.7	9.8	8.8 - 10.7	2.5‡‡‡	2.2 - 2.7	1.8***
After school	12.7	11.4 - 14.1	2.5	2.2 - 2.8	7.2	6.2 - 8.3	1.4	1.2 - 1.6	1.1***
Whole weekend day	28.1	24.8 - 31.4	2.7	2.3 - 3.0	14.2	11.8 - 16.7	1.4	1.1 - 1.6	1.3***
Morning	5.9	4.1 - 7.6	1.8	1.3 - 2.3	3.3	2.2 - 4.5	1.0	0.7 - 1.4	0.8***
Afternoon-evening	22.2	19.1 - 25.2	3.1†††	2.7 - 3.5	10.9	8.8 - 12.9	1.5††	1.2 - 1.8	1.6***

Significantly different between GAwrst % segment and AGhip % segment at *** $p < 0.001$. Significantly different between GAwrst % weekday and % weekend day at + $p < 0.05$, +++ $p < 0.001$. Significantly different between AGhip % weekday and % weekend day at + $p < 0.05$, +++ $p < 0.001$. Significantly different between GAwrst % before school – % during school – % after school at ‡‡‡ $p < 0.001$. Significantly different between AGhip % before school – % during school – % after school at ‡‡‡ $p < 0.001$. Significantly different between GAwrst % weekend morning and % afternoon-evening at ††† $p < 0.001$. Significantly different between AGhip % weekend morning and % afternoon-evening at †† $p < 0.01$, ††† $p < 0.001$.

Figure caption

Figure 1 Bland–Altman plots displaying agreement between GAwrist and AGhip derived whole weekday and whole weekend day LPA and MVPA. Note that the observed positive bias indicates that GAwrist values were higher than AGhip values. Horizontal lines represent mean bias and 95% limits of agreement.